

Kent Academic Repository

Higgs, F, Chadderton, H and Winter, SL (2011) Changes in centre of pressure measures in high and low risk fallers following six weeks of strength and balance training. In: 23rd International Society of Biomechanics Conference, July 3-7, 2011, Brussels, Belgium.

Downloaded from

https://kar.kent.ac.uk/53273/ The University of Kent's Academic Repository KAR

The version of record is available from

This document version

Publisher pdf

DOI for this version

Licence for this version

UNSPECIFIED

Additional information

Versions of research works

Versions of Record

If this version is the version of record, it is the same as the published version available on the publisher's web site. Cite as the published version.

Author Accepted Manuscripts

If this document is identified as the Author Accepted Manuscript it is the version after peer review but before type setting, copy editing or publisher branding. Cite as Surname, Initial. (Year) 'Title of article'. To be published in *Title of Journal*, Volume and issue numbers [peer-reviewed accepted version]. Available at: DOI or URL (Accessed: date).

Enquiries

If you have questions about this document contact ResearchSupport@kent.ac.uk. Please include the URL of the record in KAR. If you believe that your, or a third party's rights have been compromised through this document please see our Take Down policy (available from https://www.kent.ac.uk/guides/kar-the-kent-academic-repository#policies).



FALLS RISK EVALUATION: CENTRE OF PRESSURE COMPLEXITY VS **CLINICAL ASSESSMENT**

¹Fiona Higgs B.Sc, ^{1,2}Hugh Chadderton Ph. D and ¹Samantha L. Winter Ph. D

Department of Sport and Exercise Science, Aberystwyth University, Aberystwyth, SY23 3FD United Kingdom, ²Hywel Dda Local Health Board, UK. email: fhh09@aber.ac.uk, web: http://www.aber.ac.uk/en/sport-exercise/

Introduction:

Simple measures of centre of pressure (COP) motion can be used to predict for falls risk in older adults, e.g.: spontaneous medio-lateral (M-L) sway [1]. Reductions in complexity of COP signals have been found in older adults [4], as well as high intraclass correlation coefficients for within- and between-days across age ranges [5]. Complexity and fractility of COP signal can be quantified using specific signal processing analyses [2-4]. Comparisons between use of objective COP signal complexity and more subjective clinical measures (e.g.: multifactorial falls risk assessments) to identify falls risk have not been made.

Objective

To investigate whether measures of COP signal complexity correlate with outcome measures from clinical tests used to categorize falls patients as being at a higher or lower risk of falling. Evidencing that COP complexity, an objective measure postural stability, correlates with clinical outcomes (without requiring the administration of a battery of tests) would support the use of force plates in falls risk assessment. It is predicted that subjects categorized high risk by clinical assessment will also have reduced COP signal complexity and fractility when compared with low risk

Method - participants

A volunteer sample of twenty healthy older adults with a mean age of 78 (SD) years, height of 1.608 (SD) m, and mass of 73.46 (SD) kg. Communitydwellers attending a UK National Health Service hospital-based Falls Clinic following >1 injurious falls. The subjects were classified by a hospital doctor into a high risk group (HR) and a low risk group (LR) according scores in five keys tests (see Table 2). Subjects were referred to one of two strength and balance training programmes according to the criteria listed in Table 1.

| Five Key Tests | Scores |
|------------------------------|------------------------|
| Timed Up-and-Go-Test (TUG-T) | >.20 seconds |
| Romberg Test (RBT) | |
| Hand grip dynamometry (HGD) | Comparison to age mean |
| Timed sit-to-stand (TSTS) | |
| Falls Efficacy Scale (FES-I) | |

Table 2

Five key tests administered by Falls Clinic to categorise atients into higher and lower falls risk groups for referral to appropriate exercise intervention group

Inclusion Criteria **Exclusion Criteria** Strength and balance Acute illness deficits identified Deteriorating through scores in Five neurological condition MMSE <24 Key Tests (see Table Behaviour that creates risk to themselves or Subject willing to others undergo postural stability instruction in Unassessed syncope Unassessed low BMI strength and balance Uncontrolled exercise class tachycardia, programme hypertension or heart failure Uncontrolled diabetes or respiratory problems Uncontrolled pain 10. Untreated severe

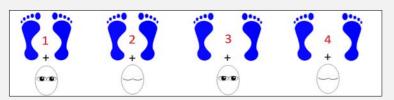
Table 1: Exclusion and Inclusion Criteria for patients entering strength and balance exercise programme

osteoporosis - T score

> -25

Method - assessment

Subjects completed balance trials in gait laboratory before and after six week training programme. Test conditions for balance trials were based on the Romberg Balance Test used in the falls clinic (see Fig. 1). Each trial lasted 20 seconds. Subjects wore their own shoes. Ground reaction force data was collected using an AMTI force plate at a sample rate of 1,000 Hz. A 4th order Butterworth filter with a low pass cut of frequency of 40Hz was applied in both directions to give zero-phase distortion. All protocols had been approved by the Dyfed-Powys National Health Service and Aberystwyth University research ethics committees. All subjects signed an informed consent document prior to participating in any testing protocols.



The four trial conditions were administered in order: 1 - narrow base eyes open (NBEO); 2 - narrow base eyes closed (NBEC); 3 - wide base eyes open (WBEO); 4 - wide base eyes closed (WBEC).

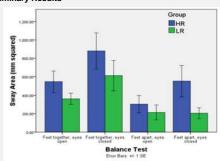
Method - data processing

Data imported into MATLAB 2009b (The Mathworks Inc., MA, USA) to compute: path length of COP; COP mean velocity, the area of the 95% best fitting ellipse, the standard deviation of the COP in the medio-lateral (ML) and anterior-posterior (AP) directions, and the median frequency and fractal dimension of the COP data in the ML and AP directions. In addition, the time dependent structure of the COP data was analysed using Approximate Entropy (ApEn) [3].

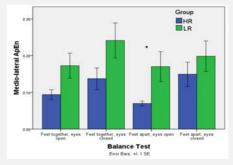
Outcome measures

A surrogate analysis of the data determined that the ApEn were due to signal properties and not measurement system noise. Statistical comparisons between types of balance trial were performed using an ANOVA, and between subject groups were performed using independent t-tests in Minitab 15 (Mintab Inc., PA, USA).

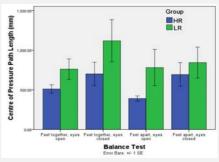
Preliminary Results



Graph 1: Sway area generally greater in HR group, but increases in both groups under eyes closed conditions except in LR group when standing on a wide BOS



Graph 2: COP complexity (ApEn) appears greater in LR group. COP complexity increases in both groups under eyes closed conditions



Graph 3: COP path length is shorter in the HR group and longest under eyes closed conditions in both groups

Conclusions

Taken together, these early results suggest it may be possible to use certain COP measures to objectively differentiate between fallers identified using a clinical tool as high and low risk. It is also possible to differentiate between the type of balance task undertaken by both groups of older adults. While the 'Five Key Test' tool in this particular setting used to distinguish between high and low risk fallers has not been validated, individual elements of the five tests have previously been used to distinguish between high and low risk fallers, and these cut off points informed development of the tool. Anecdotal evidence from the particular hospital involved in this study suggests that the 'Five Key Tests' tool was useful for specialist physical therapists and exercise professionals, however it was less successfully used by 'doorkeeper' or triage clinicians involved in referrals to these specialists. It may be at this earlier stage that simple objective tests using COP motion may be useful.

References

- Melzer I, et al., Age Ageing. 33(6):602-607, 2004.
 King MB, et al., J Gerontol. 49(6):M258-63, 1994.
- 3. Pincus SM, Proc Natl Acad Sci U S A. 88(6):2297-301, 1991.
- Duarte M, & D Sternad, Exp Brain Res. 191(3):265-76, 2008.
- 5. Lin D, et al., Gait Posture. 28(2):337-42, 2008.