

1 ANTHROPOLOGICAL SCIENCE

2 Identification of Functionally-Related Adaptations in the Trabecular Network of
3 the Proximal Femur and Tibia of a Bipedally-Trained Japanese Macaque

4
5 M. CAZENAVE^{1,2,3*}, M. NAKATSUKASA⁴, A. MAZURIER⁵, M. M. SKINNER²

6
7 ¹Division of Anthropology, American Museum of Natural History, New York, New York, USA

8 ²Skeletal Biology Research Centre, School of Anthropology and Conservation, University of
9 Kent, Canterbury, UK

10 ³Department of Anatomy, Faculty of Health Sciences, University of Pretoria, Pretoria, South
11 Africa

12 ⁴Laboratory of Physical Anthropology, Department of Zoology, Graduate School of Science,
13 Kyoto University, Kyoto, Japan

14 ⁵Institut de Chimie des Milieux et Matériaux de Poitiers (IC2MP), Université de Poitiers, UMR
15 CNRS 7285, F-86073 Poitiers, France

16

17 *Correspondence to: Marine Cazenave, Division of Anthropology, American Museum of
18 Natural History, New York, New York, USA

19 E-mail: marine.cazenave4@gmail.com

20

21 **Abstract**

22 The axial and appendicular skeleton of Japanese macaques (*Macacca fuscata*) trained to adopt
23 bipedal posture and locomotion display a number of functionally-related external and internal
24 macro- and micro-morphological changes, including site-specific cortical and trabecular bone
25 adaptations. In this study we use high-resolution microtomography scanning to analyse the 3D
26 distribution of trabecular architecture of the proximal femur and proximal tibia of *Sansuke*, a
27 male individual trained in bipedal performances for eight years, as well as five wild individuals.
28 The distribution and architecture of trabecular bone in the femoral head of *Sansuke* is distinct
29 from that found in wild *M. fuscata* individuals, with a unique bone reinforcement around the
30 region of the fovea capitis. Conversely, wild individuals exhibit two pillar-like, high-density
31 structures (converging in an inverted cone) that reach distinct regions of the posterior and
32 anterior surfaces of the femoral head. For *Sansuke*'s proximal tibia, contrary to previous
33 observations from the cortico-trabecular complex distribution at the plateau, our results do not
34 show a more asymmetric distribution between medial and lateral condyles with a medial
35 reinforcement. Additionally, relative bone volume in this region is not significantly higher in
36 *Sansuke*. However, we observed a slightly more medially placed bone reinforcement in the
37 lateral condyle compared to the wild individuals as well as a slightly higher trabecular bone
38 anisotropy in the medial than in the lateral condyle not observed in the wild individuals. These
39 analyses provide new evidence about the nature and extent of functionally-related adaptive
40 arrangements of the trabecular network at the coxofemoral and the knee joints in individuals
41 recurrently experiencing atypical load.

42

43 **Key words:** Bipedally-trained *Macaca fuscata*, Internal bone structure, Functional adaptation

44

45

Introduction

46

47 Background

48 According to the *Saru-mawashi* tradition, juvenile male Japanese macaques (*Macaca fuscata*)
49 are trained to acquire a bipedal posture and, when they can stand stably, are trained to walk for
50 2-3 km daily (~30-60 minutes in duration) while they spend the remaining time running and
51 climbing similarly to the other wild monkeys (Murasaki, 1982; Hayama, 1986; Preuschoft et
52 al., 1988). Kinematics, biomechanics and skeletal morphology in bipedal performing Japanese
53 macaques have been previously investigated, and this forced transition from solely quadrupedal
54 locomotion to the inclusion of bouts of bipedal posture has been regarded as a potentially useful
55 analogue for the evolution of human bipedalism (Hayama et al., 1992; Nakatsukasa, 2004;
56 Hirasaki et al., 2006; Ogihara et al., 2010).

57 Locomotor kinematics (Hirasaki et al., 2004; Nakajima et al., 2004; Ogihara et al., 2005,
58 2007; 2018) and energetics (Nakatsukasa, 2004, Nakatsukasa et al., 2006) in *Saru-mawashi*
59 monkeys have been studied to assess the unique dynamics associated to bipedal walking, and
60 the neurophysiology of the mechanisms of locomotor control (Mori et al., 2001, 2004, 2006;
61 Nakajima et al., 2004). During bipedal walking an increased load bearing is acting on trunk and
62 hindlimbs and there is a higher instability of the centre of mass. The hip and knee joints of
63 trained macaques are partially flexed, abducted, and laterally rotated (Okada, 1985; Nakajima
64 et al., 2004). Additionally, proximal joint angles measured in the parasagittal plane (e.g., trunk
65 and hip angles) differ between quadrupedal and bipedal gaits, whereas more distal joints (e.g.,
66 knee and ankle angles along the parasagittal plane) exhibit smaller differences. For bipedally
67 trained macaques (trained for 2-5 years to walk quadrupedally or bipedally on a motor-driven
68 treadmill), a bipedal gait requires higher but non-uniform electromyographic activity and more

69 coactivation of proximal and distal muscles than during their quadrupedal gait (Higurashi et al.,
70 2018). The duty factor (measure as the stance phase duration on the total step cycle duration)
71 also increases from a quadrupedal to bipedal gait, and the relative duration of the hindlimb
72 double-support phase increases even more (by ~20%). Proportionally longer stance and double-
73 stance phases are consistent with optimal temporal and spatial distribution of increased
74 hindlimb load (Higurashi et al., 2018).

75 In the hip, during bipedal walking of trained Japanese macaques, important compressive
76 loads are dissipated through the sacro-iliac toward the coxo-femoral joint, related to the
77 alignment between the gravitational force and the greater length of the ilium (Nakatsukasa et
78 al., 1995). The hip is generally more extended (by ~30°), and its excursion measured on a
79 parasagittal plane is smaller (of ~20°) during a bipedal versus quadrupedal gait (Higurashi et
80 al., 2018). Smaller hip excursion favours stability by limiting pitch of the upright trunk. In
81 bipedal standing, the femur is abducted and the hip joint flexed. Because of the flexed hip joint,
82 the centre of gravity is located in front of the joint, resulting in a load shift from the caudal to
83 the cranial part of the acetabulum as well as a flexing torque of the trunk about the hip. The
84 abducted femur is balanced by adducting muscles, The *m. gluteus medius*, whose activity is
85 necessary for the extension of the hip, produces an abducting moment. Major muscles that act
86 against the abducting moment are the adductors, *m. gracilis*, and hamstrings, as well as the *m.*
87 *biceps femoris*, which are all involved in the maintenance of equilibrium (Nakatsukasa et al.,
88 1995).

89 During bipedal locomotion of trained Japanese macaques, the knee is more extended and
90 laterally rotated on the femur with a valgus position, resulting in more load being directed
91 towards the medial compared to the lateral condyle (Hirasaki et al., 2004; Ogihara et al., 2009;
92 Mazurier et al., 2010). Additionally, a more extended knee joints and inverted pendulum-like
93 motion during a bipedal gait creates anterior loading of the tibial plateau (Hirasaki et al., 2004;

94 Mazurier et al., 2010). The knee angle shifts only marginally ($<10^\circ$) and its excursion in the
95 parasagittal plane remains similar ($\sim 70^\circ$) during a bipedal gait. However, its cycle-averaged
96 kinematic profile changes with maximal extension occurring just before touchdown, while the
97 knee extension seen before toe-off in a quadrupedal gait is absent during a bipedal gait
98 (Higurashi et al., 2018).

99 Several morphological and biomechanical studies have investigated the degree to which
100 different skeletal sites adapt to withstand the joint loads and stresses associated with enforced
101 bipedal standing and walking (Nakatsukasa et al., 1995; Nakatsukasa and Hayama, 2003).
102 Functionally-related external skeletal changes include the appearance of lumbar lordosis,
103 increased size of the sacroiliac and hip joints, and larger auricular surfaces (Hayama et al., 1985,
104 1986, 1992; Preuschoft et al., 1988; Nakatsukasa et al., 1995). In the hindlimb, changes include
105 posteroproximal extension of the femoral head surface, a longer axial diameter of the femoral
106 neck relative to the head-neck length, larger knee-joint surfaces, and retroflexion and
107 accentuated concavity of the tibial medial condyle (review in Nakatsukasa et al., 1995). As a
108 whole, these features reflect the causal relationships between function and adaptation of skeletal
109 morphology (e.g., Skerry, 2000; Pearson and Lieberman, 2004; Ruff et al., 2006).

110 One of the most well-studied bipedally-trained *M. fuscata* is *Sansuke*. Over a period of eight
111 years he regularly engaged in bipedal performances of 30-60 minutes that resulted in bipedal
112 walking for 2-3 km per day and spent the remaining time running and climbing similarly to the
113 other wild monkeys (Nakatsukasa and Hayama, 2003). Given the modeling response of cortical
114 and trabecular bony tissues to site-specific loading environments (Allen and Burr, 2014; Kivell,
115 2016; Barak, 2020), a number of studies have compared the bone structure of *Sansuke* to the
116 typical condition of wild Japanese macaques (Macchiarelli et al., 2001; Richmond et al., 2005;
117 Volpato et al., 2007; Mazurier et al., 2010). Based on 2D planar radiographic imaging of the
118 ilium, *Sansuke* shows an expanded dorsal bundle and a denser, more anisotropic trabecular

119 network of the iliac body as a whole as well as a thicker, vertically oriented pillar-like and
120 ventral bundle (Macchiarelli et al., 2001; Volpato et al., 2007). These results have been
121 interpreted as an adaptive response to more compressive loads dissipated through the sacroiliac
122 joint towards the coxofemoral joint, related to the alignment between the gravitational force
123 and the greater length of the ilium (Nakatsukasa et al., 1995; Volpato et al., 2007). Less distinct
124 morphostructural changes have been found in *Sansuke*'s proximal femur (Volpato et al., 2007),
125 with only minor modifications affecting the vertical bundle running from the upper head
126 towards the neck (strengthened in *Sansuke*) and the area surrounding the trochanteric fossa
127 (extended in *Sansuke*; Macchiarelli et al., 2001). Finally, a microtomographic investigation of
128 the distal femur found an increase in the degree of trabecular anisotropy in the medial condyle
129 (with a more sagittal orientation), likely reflecting the stereotypical loading that has been
130 observed in *Sansuke* compared to the wild macaque condition (Richmond et al., 2005).

131 Such evidence from the distal femur is also supported by a microtomographic study of the
132 proximal tibia, which revealed an absolutely and relatively thicker cortico-trabecular complex
133 in *Sansuke*'s articular plateau (Mazurier et al., 2010). Indeed, while the cortico-trabecular
134 complex of the medial plateau of the proximal tibia is thicker than the lateral one in both
135 *Sansuke* and wild macaques, the topographic contrast in the trained individual is much greater,
136 with marked thickening measured at the level of the anterior portion of the articular surface
137 (Mazurier et al., 2010). Also, *Sansuke*'s lateral tibial condyle shows a relatively more
138 homogeneous cortico-trabecular distribution and a slight anteroposterior thinning of the cortex.
139 This indicates greater loads acting on the medial condyle likely resulting from more laterally
140 rotated hip and knee joints (Hirasaki et al., 2004, Ogiwara et al., 2009). Biomechanically, an
141 anterior reinforcement of the tibial plateau likely plays an important role in the absorption and
142 dissipation of loads related to more extended hip and knee joints and the use of inverted
143 pendulum-like gait mechanics during bipedal locomotion (Hirasaki et al., 2004). In this study,

144 we expand on previous analyses of *Sansuke*'s skeleton with a whole-epiphysis
145 microtomographic analysis of the femoral head and proximal tibia.

146 Based on an increasing number of studies demonstrating trabecular bone modeling in
147 response to biomechanical loading during an individual's lifetime (e.g., Tsegai et al., 2013,
148 2018; Cazenave et al., 2017, 2019, 2021; Su and Carlson, 2017; Georgiou et al., 2018, 2019,
149 2020; Dunmore et al., 2019; 2020a,b; Sukhdeo et al., 2020; Bird et al., 2021, 2022; see Kivell,
150 2016 and references therein), the last two decades have seen several important conceptual and
151 technological advances in the high-resolution three-dimensional (3D) imaging, quantification
152 and statistical comparison of the internal bone structural variation (e.g., Pahr and Zysset, 2009;
153 Bondioli et al., 2010; Puymeraill, 2011; Sylvester and Terhune, 2017; DeMars et al., 2021;
154 Profico et al., 2021; Veneziano et al., 2021; Bachmann et al., 2022). However, "the confidence
155 with which internal bone structures can be used to retrodict behaviour in fossil species remains
156 a work in progress" (Almécija et al., 2021:8). Therefore, quantitative analyses of the internal
157 bone structure of joints in individuals of known behaviour can enhance our understanding of
158 the links between trabecular modeling and mechanical function, and allow stronger inferences
159 on the behaviour of fossil taxa (Biewener et al., 1996; Guldberg et al., 1997; Robling et al.,
160 2002; Mitra et al., 2005; Pontzer et al., 2006; Ruff et al., 2006; Polk et al., 2008; Barak et al.,
161 2011; Harrison et al., 2011; Christen et al., 2014). In this respect, the case of bipedally-trained
162 Japanese macaques, such as *Sansuke*, is of particular value. By using X-ray microCT and
163 cutting-edge 3D imaging techniques, we extend previous studies on *Sansuke*'s endostructural
164 bony adaptations (Macchiarelli et al., 2001; Richmond et al., 2005; Volpato et al., 2007;
165 Mazurier et al., 2010) by comparatively assessing its trabecular architecture in the proximal
166 femur and proximal tibia.

167

168 **Predictions**

169 Based on the evidence of a higher and more compressive load vertically oriented in the
170 caudal region of the acetabulum during bipedal posture and gait in trained macaques, and on
171 the assumption that the trabecular bone of the femoral head is sensitive enough to model
172 according to the loading conditions during the bipedal posture and locomotion in *Sansuke* (that
173 only represent a short amount of time in the daily life of *Sansuke*) as seen in the pelvic bone
174 (Volpato et al., 2007), in *Sansuke*'s femoral head we predict a pattern of trabecular architecture
175 that is distinct from that found in wild *M. fuscata*. Specifically, being characterized by an
176 approximately superoinferiorly-oriented bone reinforcement resulting from more vertical
177 loading at the proximal femoral head during bipedal locomotion. This will be associated with
178 higher relative bone volume, thicker trabeculae and a higher degree of anisotropy in *Sansuke*
179 (Nakatsukasa et al., 1995, Volpato et al., 2007).

180 Based on the evidence of a more pronounced medial loading in the tibial articular surface
181 compared with the lateral plateau resulting from the more laterally rotated tibia on the femur
182 (Hirasaki et al., 2004, Ogihara et al., 2009), as well as, anterior loading related to a more
183 extended hindlimb joint and the use of an inverted pendulum-like motion during bipedal
184 locomotion (Hirasaki et al., 2004), compared to the typical condition of wild individuals, in
185 *Sansuke* we expect to find: (i) a more asymmetric distribution in relative bone volume between
186 the medial and the lateral condyles that is associated with an increase in the anterior region of
187 the medial condyle, and (ii) greater bone volume fraction associated with a higher degree of
188 anisotropy. This expectation is based on the assumption that the trabecular bone of the proximal
189 tibia is sensitive enough to model according to the loading conditions during the bipedal posture
190 and locomotion in *Sansuke* (that only represent a short amount of time in the daily life of
191 *Sansuke*) as seen in the cortico-trabecular complex of the tibial plateau (Mazurier et al., 2010).

192

193

Material and Methods

194

195 We investigated the left and right proximal femora and tibiae of *Sansuke*, a 10-kg male *M.*
196 *fuscata* engaged in bipedal performances lasting 30-60 minutes/day (Murasaki, 1982; Hayama,
197 1986; Preuschoft et al., 1988) from the age of 2 years until his death that occurred at 10 years
198 (Nakatsukasa and Hayama, 2003). The comparative sample consists of five right proximal
199 femora (from 4 likely male and 1 likely female individuals, based on skeletal size) and five
200 right proximal tibiae (all likely male, based on skeletal size) from non-bipedally trained wild
201 individuals of the same taxon. Four of the five femora and tibiae are associated. All specimens
202 lack macroscopic evidence of alteration or pathological changes, and are housed at the
203 Laboratory of Physical Anthropology, Kyoto University (Japan). Details on the composition of
204 the sample are provided in Table S1.

205 *Sansuke's* femora and tibiae and one femur and two tibiae from wild individuals were
206 scanned in 2005 by synchrotron radiation microtomography (SR- μ CT) at the European
207 Synchrotron Radiation Facility (ESRF) medical beam line ID17, Grenoble (details in Mazurier
208 et al., 2010). The voxel size of the reconstructed volume is $45.5 \times 45.5 \times 43.6$ microns (μm).
209 The remaining sample (four femora and three tibiae) were scanned in 2022 at the Laboratory
210 of Physical Anthropology, Kyoto University, using a ScanXmate A080s (Comscan co.) with an
211 isotropic voxel size of $41.9 \mu\text{m}$, for the proximal femora, and ranging from $54.6 \mu\text{m}$ to $59.0 \mu\text{m}$,
212 for the proximal tibiae (Table S1).

213 All specimens were virtually reoriented in Avizo v.9.0 software (Visualization Sciences
214 Group Inc., Bordeaux) using a landmarking-based automatic alignment. The proximal femora
215 were then virtually cut at the head-neck junction and the tibia at the level of the tuberosity
216 perpendicular to the main axis of the proximal portion of the shaft.

217 All oriented bones were segmented using the MIA-Clustering segmentation (Dunmore et al.,
218 2018) to automatically isolate bone from air and then processed with Medtool 4.6

219 (<http://www.dr-pahr.at>). In Medtool 4.6, we followed the procedure detailed in Gross et al.
220 (2014) and Tsegai et al. (2018). First, the whole bone was segmented by a ‘fill’ operation that
221 casts rays from the outer cortical shell at multiple angles followed by a morphological closing
222 step. A series of morphological filters were then applied to identify and remove the cortical
223 shell, thus isolating the trabecular structure. A 3D background grid with node spacing of 2.5
224 mm was superimposed on the isolated trabecular volume and overlapping spherical volumes of
225 interest (VOI), 5 mm in diameter, were centred at each of its nodes. Trabecular bone volume
226 fraction (BV/TV), trabecular thickness (Tb.Th.), trabecular spacing (Tb.Sp.), and degree of
227 anisotropy (DA) were measured in each VOI and the values interpolated on the centroids of a
228 3D tetrahedral mesh of the trabecular volume created with the Computational Geometry
229 Algorithms Library. Morphometric maps of the distribution of each parameter can then be
230 visualized (additional technical details in Tsegai et al., 2018).

231 Statistical analyses were performed in RStudio v. 1.2.5033 running with R v. 3.4.4 (R Core
232 Team, 2018). Plots were generated using ggplot2 (Wickham, 2009). Standardized measures
233 were calculated for interspecific comparisons, in which for each individual the raw values of
234 each parameter were divided by the individual mean of all values of this parameter. For each
235 standardized parameter, the significance of the two-by-two individual differences was tested by
236 the non-parametric pairwise Wilcoxon rank sum tests with a Bonferroni correction as well as
237 two-sample t-test via Monte Carlo sampling with 1000 permutations. Given that for each
238 specimen a set of hundreds of VOIs is extracted sampling the whole bone, with four variables
239 measured in each VOI, pairwise Pearson correlation tests between the four variables have been
240 conducted for each specimen. These tests aim to measure, for each specimen, the degree of
241 correlation between the distributions throughout the bone of the investigated parameters.
242 Following Chan (2003), $r > 0.8$ shows a high correlation, $0.6 < r < 0.8$ shows a moderate

243 correlation and $r < 0.6$ shows a poor correlation. A significance threshold of 0.05 for the p -
244 values was adopted for all statistical analyses.

245

246 **Results**

247

248 **Proximal femur**

249 Figure 1 presents morphometric maps in medial view of the distribution of the four
250 investigated trabecular parameters (BV/TV, Tb.Th., Tb.Sp. and DA) in *Sansuke*'s left and right
251 femoral heads in comparison to those from a wild macaque. The maps of the remaining wild
252 individuals are shown in the online Supplementary Material Figure S1 and the same results in
253 superior view for all individuals are presented in Figure S2. As predicted, in *Sansuke* there is a
254 distinct pattern of bone distribution from that found in the wild *M. fuscata* individuals. However,
255 the expectation of an approximately superoinferiorly-oriented bone reinforcement is not
256 detected. Indeed, in both *Sansuke*'s femoral heads, the BV/TV distribution indicates a
257 reinforcement that is limited to the region of the fovea capitis. Conversely, in KAS 266 and
258 KAS 276 (Figure 1 and Figure S1, S2) two concentrations of relatively higher BV/TV values
259 forming two converging pillar-like structures are found in the posterior and anterior surfaces of
260 the head, respectively. In the other three individuals (KAS 269, KAS281 and KAS 284; Figure
261 S1, S2), such structures appear as less discrete units, with a continuous concentration of bone
262 density spanning in the superior aspect of the femoral head.

263 In *Sansuke*, Tb.Th. distribution matches the BV/TV arrangement, with a concentration of
264 high Tb.Th. values in the region of the fovea capitis, while in the wild individuals a high
265 concentration of Tb.Th. tends to be observed in the posterosuperior surface. However, in this
266 case, for the wild specimens, there is no concentration of high Tb.Th. at the level of the anterior
267 BV/TV pillar-like structure, and the posterosuperior concentration of high Tb.Th. does not

268 extend internally but is confined to the subchondral layers (except for KAS 276 showing a thin
269 extension of high Tb.Th. toward the neck in the posterior region of the head). In both *Sansuke*
270 and the comparative sample, Tb.Sp. tends to show lower values on the inferoanterior aspect of
271 the head, while the highest values of DA tend to be found in the head-neck junction, even though
272 the signal in *Sansuke* is less evident. In some wild individuals, an extension of the distribution
273 of the highest DA values in the anterior and posterior surfaces is observed.

274 Our prediction of overall higher bone density and thicker struts in *Sansuke* cannot be
275 supported by our results. In *Sansuke*'s right femoral head, pairwise Wilcoxon tests show that
276 both variables differ statistically from those measured in three wild individuals (KAS 266, KAS
277 281, KAS 284) for BV/TV and one wild individual (KAS 266) for Tb.Th. (Figure 2, Table S2).
278 However, in *Sansuke*'s left femoral head, no appreciable differences with the wild sample have
279 been found for BV/TV and Tb.Th. In addition, the Monte-Carlo permutation tests show no
280 differences for all parameters and all pairwise comparisons. Figure 2 illustrates that the medians
281 of both *Sansuke*'s femoral head BV/TV and Tb.Th. are slightly lower than of the wild sample.
282 It is nonetheless interesting to note that in this trained individual we observe the highest absolute
283 BV/TV and relative BV/TV and Tb.Th. values in individual VOIs of the entire sample (Figures
284 1, 2). These high values are from the VOIs extracted at the region of the fovea capitis. No
285 appreciable differences have been found for DA and Tb.Sp. (Figure 2, Table S2).

286 The distribution patterns of trabecular parameters shown by the morphometric maps is
287 supported by the correlation tests presented in Table 1. In both *Sansuke*'s femora and in the
288 wild male KAS 269, BV/TV and Tb.Th. are highly correlated ($r > 0.8$; Chan, 2003), which is
289 not the case in the other comparative specimens that show a moderate correlation ($0.6 < r < 0.8$).
290 In *Sansuke*, a functionally-related bone reinforcement at the region of the fovea capitis seems
291 to be achieved through thickening the trabecular struts. Additionally, in *Sansuke* DA is
292 moderately correlated with BV/TV and it is highly and moderately correlated with Tb.Th. for

293 the left and right femora, respectively. All other tests show poor correlation ($r < 0.6$). All
294 Pearson correlation coefficients are statistically significant ($p\text{-value} \leq 0.05$) except for
295 coefficients equal to or lower than 0.1 for which interpretation of the results cannot be certain.

296

297 **Proximal tibia**

298 The distribution maps of the four trabecular parameters assessed in *Sansuke*'s left and right
299 proximal tibiae are presented in Figure 3 and compared to those from a wild macaque (n.b.,
300 maps of the other four wild individuals are shown in Figure S3). In this case, the results do not
301 follow our first prediction. In *Sansuke*, the BV/TV distribution does not show a clear asymmetry
302 between medial and lateral condyles, nor an anterior structural reinforcement across the whole
303 plate. Indeed, a similar pattern of BV/TV, Tb.Sp. and DA distribution is found in all individuals.
304 Specifically, all investigated proximal tibiae show (i) a concentration of high BV/TV in the
305 medial area of the medial condyle and in the central area of the lateral condyle (even though
306 the bone reinforcement in the lateral condyle is slightly more medially placed in *Sansuke*,
307 notably in the left tibia, than in the wild individuals); (ii) the lowest Tb.Sp. values in the
308 posterior area of the articular surface; and (iii) a concentration of high DA values in the central
309 region of the posterior portion. However, the medial condyle tends to be more anisotropic (i.e.,
310 higher DA) than the lateral condyle in *Sansuke*, while no asymmetrical distribution of DA is
311 observed in the wild individuals. Moreover, no clear trend can be identified for Tb.Th.
312 distribution apart from highest Tb.Th. values observed in the central intercondylar area and the
313 posterior surface of the proximal diaphysis in *Sansuke*, KAS 276 and KAS 309. Contrary to our
314 second prediction, bone volume fraction and degree of anisotropy are not significantly higher
315 in *Sansuke* than in the wild *M. fuscata* individuals (Figure 4; Table S3). The permutation Monte
316 Carlo tests show no differences for all parameters and all pairwise comparisons.

317 These qualitative observations are confirmed by the correlation tests presented in Table 2.
318 In all individuals, BV/TV is highly negatively correlated with Tb.Sp. ($r > 0.8$) except for KAS
319 269, which shows a moderate correlation ($0.6 < r < 0.8$) between the two parameters. BV/TV
320 is highly correlated with Tb.Th. in the right femur of *Sansuke* and KAS 269, and moderately
321 correlated with Tb.Th. in *Sansuke* left femur and all wild individuals, except KAS 276, which
322 shows a poor correlation ($r < 0.6$). Finally, in *Sansuke*, but not in all wild individuals, Tb.Th. is
323 negatively moderately or highly correlated with DA. All other tests show poor correlations. All
324 Pearson correlation coefficients are statistically significant (p -value ≤ 0.05), except for
325 coefficients equal to or lower than 0.1. Differences in voxel size between the scans might affect
326 the strength of correlations between *Sansuke* and comparative sample.

327

328 **Discussion and Conclusions**

329

330 An increasing number of studies have tested the degree to which variation in trabecular bone
331 structure at different skeletal sites reflects differences in locomotor-related loadings in humans
332 and other primates (review in Kivell, 2016). For instance, although the link between the
333 endostructural architecture of the proximal femur and load transfer and dissipation is more
334 complex than assumed by the first mechanical models (e.g., Fajardo et al., 2007; Ryan and
335 Walker, 2010; Shaw and Ryan, 2012), trabecular bone variation in the primate femoral head
336 has provided clear evidence for structural differences across locomotor groups (Fajardo and
337 Müller, 2001; MacLatchy and Müller, 2002; Ryan and Ketcham, 2002a, b, 2005; Ryan and
338 Krovitz, 2006; Saporin et al., 2011; Ryan and Shaw, 2012, 2015; Raichlen et al., 2015; Ryan et
339 al., 2018; Tsegai et al., 2018; Georgiou et al., 2019; Cazenave et al., 2020).

340 In 2019, a study of trabecular bone structural distribution patterns of the extant great ape
341 femoral head using a whole epiphysis approach similar to that of the present study, first revealed

342 that holistic evaluations of the trabecular architecture show patterns linked to locomotor
343 behaviour (Georgiou et al., 2019). More precisely, *Pan* and *Gorilla* demonstrated two
344 concentrations of higher bone density - one in the posterosuperior aspect and one in the anterior
345 portion of the femoral head - consistent with hip orientation and joint loading during two main
346 locomotor modes: knuckle-walking and climbing. These two pillar-like structures extend and
347 converge internally. In *Pongo*, these structures are less evident as discrete units with bone
348 density concentrated as a band across the superior aspect of the femoral head and interpreted as
349 reflecting less discrete and more homogenous loading of the hip joint during arboreal
350 locomotion (Georgiou et al., 2019, 2020). In terms of general bone density of the femoral head,
351 the five wild *M. fuscata* individuals represented in our study show an ape-like trabecular
352 conformation, but with some variation. Indeed, two specimens show two well-distinct pillars,
353 while the other three femora display less discrete pillar-like structures arising from the superior
354 head surface but merged within a topographically nearly homogeneous network. Such
355 endostructural arrangement is consistent with the postural and locomotor modes typical of wild
356 Japanese macaques, which are quadrupeds terrestrially, but also arboreal, with vertical climbing
357 and short distance leaping (Negayama, 1983; Kimura, 1985; Okada, 1985; Nakano, 1996;
358 Nakano et al., 1996; Chatani, 2003; Fleagle, 2013). They have developed hamstring muscles
359 which function to extend hip joints to propel the body forward (Haxton, 1947; Kimura et al.,
360 1979). Similar to the condition displayed by *Pan* and *Gorilla*, in *M. fuscata* the hip is flexed
361 during the swing phase of quadrupedalism, with a maximum flexion angle of $\sim 45^\circ$ and a mobile
362 (excursion) range of the hip joint of about $\sim 65^\circ$ during a single step cycle (Nakajima et al.,
363 2004). This is consistent with high loading of the posterosuperior region of the femoral head
364 and the relatively higher bone density found in this region. During the resting posture, vertical
365 climbing and leaping, the hip is highly flexed (Hirasaki et al., 1993; Isler, 2005), which would
366 result in the anterior aspect of the head contacting the lunate surface of the acetabulum. In the

367 wild specimens examined in our study, while the posterosuperior subchondral bone
368 reinforcement is accompanied by thicker struts, this is not the case for an anterior reinforcement.
369 As a whole, these results indicate that additional investigations are needed for a better
370 understanding of the functional significance of the intra-individual topographic variation of the
371 femoral head trabecular network in extant primates displaying different locomotor modes, and
372 especially of the direct links between hypothesized load environment and site-specific
373 microstructural arrangement. A future area of investigation would be finite element analyses
374 (FEA) and in particular inverse-bone remodelling (Synek et al., 2019) and homogenized FE
375 (Bachmann et al., 2022) that are sensitive enough to detect differences in external joint loadings
376 in primates from bone microarchitectures.

377 In agreement with our first two predictions, *Sansuke*'s femoral head does show a global
378 pattern of bone density and trabecular thickness distribution distinct from the wild macaque
379 condition. However, contrary to our expectation based on a previous analysis of the iliac
380 textural characteristics (Volpato et al., 2007), *Sansuke* does not show a developed
381 superoinferior bone reinforcement resulting from more vertical loading at the proximal femoral
382 head occurring during bipedal performances, and overall BV/TV and Tb.Th. values do not
383 discriminate *Sansuke* from the wild macaques. Given that *Sansuke*'s main activities are running
384 and climbing as wild macaques, this result questioned whether the trabecular bone of the
385 femoral head might have been sensitive enough to model according to the loading conditions
386 encountered during bipedal activities and that trabecular bone architecture of the femoral head
387 does not only reflect the less stereotyped and multiaxial loading conditions of a wild-like
388 locomotor behaviour. Nonetheless, a concentration of high bone density along with thick struts
389 is uniquely found in *Sansuke* in the region of the fovea capitis, the nonarticular depression
390 providing attachment to the ligamentum teres.

391 In humans, the ligamentum teres mainly carries out a stabilizing function of the hip joint
392 (Rao et al., 2001; Philippon et al., 2014; O'Donnell and Arora, 2018), but also limits hip
393 adduction during a bipedal gait (Kaplan, 1949; Delcamp et al., 1988; Gray and Villar, 1997;
394 Rao et al., 2001; Demange et al., 2007; Kapandji, 2011; Villar and Santori, 2012; van Arkel et
395 al., 2015; O'Donnell et al., 2018). In *Sansuke*, rather than a pillar-like structure superoinferiorly
396 crossing the femoral head, a bone reinforcement in the region of the insertion of the fovea capitis
397 might represent the functionally-related structural response to the need of stabilizing the hip
398 joint during the bipedal-like trained cycle in relation to the recurrent instances of adduction
399 (Nakatsukasa et al., 1995; Ogihara et al., 2009, 2018), and is associated to the posteroproximal
400 extension of his femoral head surface (Nakatsukasa et al., 1995).

401 While locomotor-related variation of the proximal femur inner architecture has received
402 considerable attention, the endostructural signal of the proximal tibia, has been focused on
403 human clinical studies (Ritter et al., 2014; Burnett, 2017; Roberts et al., 2017; Renault et al.,
404 2020; Goliath et al., 2022) and remains poorly investigated in non-human extant primates and
405 fossil hominins (Ahluwalia, 2000; Mazurier 2006; Mazurier et al., 2010).

406 Comparative functional anatomy shows that the mammalian knee is “an alarmingly complex
407 joint” (Lovejoy, 2007: 326). In the primate proximal tibia, variation exists in size and shape of
408 the medial and lateral articular surfaces and the proportions of the intercondylar tubercles of
409 the plateau (Tardieu, 1983; Lovejoy, 2007), reflecting adaptations to a wide range of postural
410 and locomotor modes (Aiello and Dean, 1990). Accordingly, comparative and experimental
411 investigations on the endostructural arrangement of the proximal tibia in extant primate taxa
412 have the potential of providing a valuable framework for interpreting the internal bone
413 condition from fossil hominin specimens (Mazurier, 2006; Mazurier et al., 2010).

414 In *Sansuke*, none of the expectations based on the evidence of a thicker cortico-trabecular
415 complex heterogeneously distributed beneath the articular surface of the proximal tibia

416 (Mazurier, 2006; Mazurier et al., 2010) are supported by our analyses. *Sansuke* does not show
417 an average higher bone density compared to the wild macaques, nor the highest bone density
418 values. Additionally, we could not identify a greater degree of asymmetry in trabecular bone
419 volume distribution between the two condyles compared to the wild individuals, and no
420 trabecular variables are distinct. However, in *Sansuke*'s tibia there is a slightly more medially
421 placed subtle bone reinforcement in the lateral condyle compared to the wild individuals, as
422 well as, slightly higher trabecular bone anisotropy in the medial condyle that is not observed in
423 the wild individuals. This is consistent with the more anisotropic medial femoral condyle
424 compared to the lateral one identified in *Sansuke* (Richmond et al., 2005).

425 Within the current knowledge on metabolic differences and trade-offs between cortical and
426 trabecular tissues through life, including during ontogeny, these discrepancies between the clear
427 adaptations at the proximal tibia observed in *Sansuke*'s cortico-trabecular complex adjustment
428 (Mazurier et al., 2010) and the less distinct structural changes at the underlying trabecular
429 network are unexpected. Under experimental analyses the human tibial shaft (Erlandson et al.,
430 2012; Weatherholt et al., 2013; Murray et al., 2022; for other skeletal elements see also
431 Kontulainen et al., 2002; Eser et al., 2009; Erlandson et al., 2012) and mouse tibial shaft (De
432 Souza et al., 2005; Brodt and Silva, 2010) show that cortical bone is primarily reflecting early
433 life behaviour, while epiphyseal trabecular bone microarchitecture may primarily be reflecting
434 adult loading. This is consistent with a recent study by Saers et al. (2022) showing an adult-like
435 trabecular structure in the calcaneum of 1.5-2 year Japanese macaques that recently adopted an
436 adult-like locomotion (Saers et al., 2022). Noting that *Sansuke* started bipedal training at the
437 adult age of two years (Nakatsukasa and Hayama, 2003), we would expect that in its tibial
438 proximal epiphysis cortical bone thickness would reflect early life wild behaviour, and the
439 trabecular structure would be modeled based on adaptations to bipedal loading. Therefore, in
440 addition to adding information to the discussion about trade-offs between cortical and trabecular

441 tissue throughout life and notably between young and adulthood, our results raise questions
442 about differences in site-specific functional adaptations and notably possible differences
443 between epiphyseal (articular) and diaphyseal cortical adaptations.

444 In the present case, discrepancies in the functional signal between the subchondral cortico-
445 trabecular complex and trabecular tissue of the tibial plateau might reflect differences in
446 sensitivity to the local loading environment during bipedal performances, where the
447 subchondral layers sufficiently withstand and counteract the loads occurring at the knee because
448 of the bipedal training, with no evident impact on the conformation of the deeper trabecular
449 bone. Indeed, in humans it has been demonstrated that the proximal tibia cartilage (including
450 the menisci) and its supporting subchondral bone have corresponding mechanical functions
451 (Lereim et al., 1974; Duncan et al., 1987; Odgaard et al., 1989; Milz and Putz, 1994; McKinley
452 and Bay, 2001; Hoemann et al., 2012) and that the subchondral region exhibits strong
453 architectural response to differences in joint loading regimes (Pontzer et al., 2006; Goliath et
454 al., 2022). In the human patella, another component of the knee joint, a similarly functionally-
455 related heterogeneous distribution of the subchondral bone gradually disappears with depth,
456 with most of the deeper trabecular network lacking site-specific structural adaptations (Hoechel
457 et al., 2015). However, while studies have revealed variations of the topographic distribution
458 of the cortico-trabecular complex thickness related to differences in locomotor-related loading
459 environment at the knee joint between primates (Ahluwalia, 2000; Mazurier, 2006; Mazurier et
460 al., 2010), we still lack enough comparative evidence about the endostructural conformation of
461 this skeletal site in extant primates revealing any possible link between locomotor mode(s) and
462 site-specific network variation of the trabecular bone beneath the cortico-trabecular complex.

463 Intraspecific variations in lower limb trabecular bone between populations experiencing
464 different level of activities and various loading modalities have been investigated in human
465 populations (Stock, 2006; Ryan and Shaw, 2015; Chirchir et al., 2015, 2017; Saers et al., 2016,

466 2021; Doershuk et al., 2018; Mulder et al., 2019). First, localized response to loading, rather
467 than systemic variation, is the main driver of these population differences (Chirchir et al., 2017;
468 Doershuk et al., 2018). In addition, all studies showed that on the lower limb, high levels of
469 physical activity contribute to increase bone strength achieved through an increase in bone
470 volume fraction and trabecular thickness. In the case of the present study, while bipedally-
471 trained macaques experience an increase in vertical loading at the hip and knee joints during
472 bipedal standing and walking, we did not identify a higher bone volume and trabecular
473 thickness compared to the condition observed in wild individuals. It is, therefore, important to
474 recall here that the trained macaques spend most of the time running and climbing similar to
475 the other wild monkeys (Nakatsukasa et al., 1995; Hirasaki et al., 2004), thus experiencing
476 postural/locomotion-related multiaxial loads. In the case of *Sansuke*, trained from the age of
477 two, a wild behaviour was adopted during childhood. Even though morphological local
478 modifications have been identified in *Sansuke*'s outer and inner skeleton in response to bipedal-
479 related constraints (Nakatsukasa et al., 1995; Volpato et al., 2007; Mazurier et al., 2010), the
480 frequency as well as nature of loading locally acting on hip and knee joint in *Sansuke* during
481 bipedal posture and locomotion against the backdrop of the entire behavioral profile to evoke
482 an osseous response.

483 In conclusion, the high-resolution non-invasive analysis of the postcranial skeleton of a
484 bipedally-trained Japanese macaque, *Sansuke*, continues to provide direct evidence about the
485 rheological and adaptive characteristics of mechanosensitive bony tissues when intermittently
486 facing atypical load related to relatively short but recurrent changes in joint loading
487 environment. In this specific case, the comparative assessment of the functionally-related
488 adjustment of the trabecular network at the femoral head (coxofemoral joint) and the proximal
489 tibia (knee joint) provides new original and partially unexpected results, including on the
490 patterns of network variation characterizing the wild macaque representatives used for

491 comparison. Our results are relevant to attempts to predict and infer locomotory behaviour in
492 fossil primates, including those such as hominins that are defined by the adoption of bipedal
493 locomotion.

494

495 **Acknowledgements**

496 Acquisitions of *Sansuke's* femora and tibiae and of one femur and two tibiae from wild
497 macaques were performed at the ESRF (France) in collaboration with V. Volpato (Univ.
498 Poitiers) within the EC TNT project led by R. Macchiarelli (Univ. Poitiers and MNHN, Paris).
499 The remaining specimens were detailed at the Laboratory of Physical Anthropology, Kyoto
500 University, in collaboration with Suo Sarumawashi (Suo Monkey Performance Association)
501 and we are grateful of N. Morimoto (Kyoto Univ.) for taking CT scans of these specimens. For
502 discussion, we thank A. Bardo (MNHN, Paris), C. Dunmore (Univ. Kent), T. Kivell (Univ.
503 Kent), Z. Tsegai (Univ. Kent, Canterbury), C. Zanolli (PACEA, Bordeaux). Finally, we are
504 grateful to Hiroko Oota, the Associate Editor and to two anonymous reviewers for constructive
505 comments that considerably improved this manuscript. M.C. was funded by the Fyssen
506 Foundation and the Division of Anthropology of the American Museum of Natural History,
507 New York. This project has received funding from the European Research Council (grant
508 agreement No. 819960).z

509

510 **References**

511 Ahluwalia K. (2000) Knee joint load as determined by tibial subchondral bone density: its
512 relationship to gross morphology and locomotor behavior in catarrhines. PhD Thesis, State
513 University of New York, Stony Brook.

514 Aiello L., Dean C. (1990) An introduction to human evolutionary anatomy. Academic Press,
515 New York.

516 Allen M.R., Burr D.B. (2014) Bone modeling and remodeling. In: Basic and Applied Bone
517 Biology. Academic Press, London, pp. 75-90

518 Almécija S., Hammond A.S., Thompson N.E., Pugh K.D., Moyà-Solà S., Alba D.M. (2021)
519 Fossil apes and human evolution. *Science*, 372: eabb4363.

520 Bachmann S., Dunmore C.J., Skinner M.M., Pahr D.H., Synek A. (2022) A computational
521 framework for canonical holistic morphometric analysis of trabecular bone. *Scientific*
522 *reports*, 12: 1-13.

523 Barak M.M. (2020) Bone modeling or bone remodeling: That is the question. *American Journal*
524 *of Physical Anthropology*, 172: 153-155.

525 Barak M.M., Lieberman D.E., Hublin J.J. (2011) A Wolff in sheep's clothing: Trabecular bone
526 adaptation in response to changes in joint loading orientation. *Bone*, 49: 1141-1151.

527 Biewener A.A., Fazzalari N.L., Konieczynski D.D., Baudinette R.V. (1996) Adaptive changes
528 in trabecular architecture in relation to functional strain patterns and disuse. *Bone*, 19: 1-8.

529 Bird E.E., Kivell T.L., Skinner M.M. (2021) Cortical and trabecular bone structure of the
530 hominoid capitate. *Journal of Anatomy*, 239: 351-373.

531 Bird E.E., Kivell T.L., Skinner M.M. (2022) Patterns of internal bone structure and functional
532 adaptation in the hominoid scaphoid, lunate, and triquetrum. *American Journal of Biological*
533 *Anthropology*, 177: 266-285.

534 Bondioli L., Bayle P., Dean C., Mazurier A., Puymeraill L., Ruff C., Macchiarelli R. (2010)
535 Morphometric maps of long bone shafts and dental roots for imaging topographic thickness
536 variation. *American Journal of Physical Anthropology*, 142: 328-334.

537 Brodt M.D., Silva M.J. (2010) Aged mice have enhanced endocortical response and normal
538 periosteal response compared with young-adult mice following 1 week of axial tibial
539 compression. *Journal of Bone and Mineral Research*, 25: 2006-2015.

540 Burnett J.K. (2017) Bone strain change as a result of a long distance run modeled on a finite
541 element tibia. PhD Dissertation, Iowa State University.

542 Cazenave M., Braga J., Oettlé A., Pickering T.R., Heaton J.L., Nakatsukasa M., Thackeray F.J.,
543 de Beer F., Hoffman J., Dumoncel J., Macchiarelli R. (2019) Cortical bone distribution in
544 the femoral neck of *Paranthropus robustus*. *Journal of Human Evolution*, 135: 102666.

545 Cazenave M., Braga J., Oettlé A., Thackeray J.F., De Beer F., Hoffman J., Endalama E., Redae
546 B.E., Puymeraill L., Macchiarelli R. (2017) Inner structural organization of the distal
547 humerus in *Paranthropus* and *Homo*. *Comptes Rendus Palevol*, 16: 521-532.

548 Cazenave M., Oettlé A., Pickering T.R., Heaton J.L., Nakatsukasa M., Thackeray J.F., Hoffman
549 J., Macchiarelli R. (2021) Trabecular organization of the proximal femur in *Paranthropus*
550 *robustus*: Implications for the assessment of its hip joint loading conditions. *Journal of*
551 *Human Evolution*, 153: 102964.

552 Chan Y.H. (2003) Biostatistics 104: correlational analysis. *Singapore Medical Journal*, 44: 614-
553 619.

554 Chatani K. (2003) Positional behavior of free-ranging Japanese macaques (*Macaca fuscata*).
555 *Primates*, 44: 13-23.

556 Chirchir H., Kivell T.L., Ruff C.B., Hublin J.J., Carlson K.J., Zipfel B., Richmond B.G. (2015)
557 Recent origin of low trabecular bone density in modern humans. *Proceedings of the National*
558 *Academy of Sciences*, 112: 366-371.

559 Chirchir H., Ruff C.B., Junno J.A., Potts R. (2017) Low trabecular bone density in recent
560 sedentary modern humans. *American Journal of Physical Anthropology*, 162: 550-560.

561 Christen P., Ito K., Ellouz R., Boutroy S., Sornay-Rendu E., Chapurlat R.D., Van Rietbergen
562 B. (2014) Bone remodelling in humans is load-driven but not lazy. *Nature communications*,
563 5: 1-5.

564 De Souza R.L., Matsuura M., Eckstein F., Rawlinson S.C.F., Lanyon L.E., Pitsillides A.A.
565 (2005) Non-invasive axial loading of mouse tibiae increases cortical bone formation and
566 modifies trabecular organization: A new model to study cortical and cancellous
567 compartments in a single loaded element. *Bone*, 37: 810-818.

568 Delcamp D.D., Klaaren H.E., van Meerdervoort H.P. (1988) Traumatic avulsion of the
569 ligamentum teres without dislocation of the hip. Two case reports. *Journal of Bone and Joint*
570 *Surgery*, 70: 933-935.

571 Demange M.K., Kakuda C.M.S., Pereira C.A.M., Sakaki M.H., Albuquerque R.F.M. (2007)
572 Influence of the femoral head ligament on hip mechanical function. *Acta Ortopedica*
573 *Brasileira*, 4: 187-190.

574 DeMars L.J., Stephens N.B., Saers J.P., Gordon A., Stock J.T., Ryan T.M. (2021) Using point
575 clouds to investigate the relationship between trabecular bone phenotype and behavior: An
576 example utilizing the human calcaneus. *American Journal of Human Biology*, 33: e23468.

577 Doershuk L.J., Saers J.P.P., Shaw C.N., Jashashvili T., Carlson K.J., Stock J.T., Ryan T.M.
578 (2018) Complex variation of trabecular bone structure in the proximal humerus and femur
579 of five modern human populations. *American Journal of Physical Anthropology*, 168: 104-
580 118.

581 Duncan H., Jundt J., Riddle J.M., Pitchford W., Christopherson T. (1987) The tibial
582 subchondral plate. A scanning electron microscope study. *The Journal of Bone and Joint*
583 *Surgery*: 69, 1212-1220.

584 Dunmore C.J., Bardo A., Skinner M.M., Kivell, T.L. (2020a) Trabecular variation in the first
585 metacarpal and manipulation in hominids. *American Journal of Physical Anthropology*, 171:
586 219-241.

587 Dunmore C.J., Kivell T.L., Bardo A., Skinner M.M. (2019) Metacarpal trabecular bone varies
588 with distinct hand-positions used in hominid locomotion. *Journal of Anatomy*, 235: 45-66.

589 Dunmore C.J., Skinner M.M., Bardo A., Berger L.R., Hublin J.J., Pahr D.H., Kivell T.L.
590 (2020b) The position of *Australopithecus sediba* within fossil hominin hand use diversity.
591 Nature Ecology & Evolution, 4: 911-918.

592 Dunmore C.J., Wollny G., Skinner M.M. (2018) MIA-Clustering: a novel method for
593 segmentation of paleontological material. PeerJ, 6: e4374.

594 Erlandson M., Kontulainen S., Chilibeck P., Arnold C., Faulkner R., Baxter-Jones A. (2012)
595 Higher premenarcheal bone mass in elite gymnasts is maintained into young adulthood after
596 long-term retirement from sport: A 14-year follow-up. Journal of Bone and Mineral
597 Research, 27: 104-110.

598 Eser P., Hill B., Ducher G., Bass S. (2009) Skeletal benefits after long-term retirement in former
599 elite female gymnasts. Journal of Bone and Mineral Research, 24: 1981-1988.

600 Fajardo R.J., Müller R. (2001) Three-dimensional analysis of nonhuman primate trabecular
601 architecture using micro-computed tomography. American Journal of Physical
602 Anthropology, 115: 327-336.

603 Fajardo R.J., Müller R., Ketcham R.A., Colbert M. (2007) Nonhuman anthropoid primate
604 femoral neck trabecular architecture and its relationship to locomotor mode. Anatomical
605 Record, 290: 422-436.

606 Fleagle J.G. (2013) Primate adaptation and evolution. Academic press, New York.

607 Georgiou L., Dunmore C.J., Bardo A., Buck L.T., Hublin J.J., Pahr D.H., Skinner M.M. (2020)
608 Evidence for habitual climbing in a Pleistocene hominin in South Africa. Proceedings of the
609 National Academy of Sciences, 117: 8416-8423.

610 Georgiou L., Kivell T.L., Pahr D.H., Buck L.T., Skinner M.M. (2019) Trabecular architecture
611 of the great ape and human femoral head. Journal of Anatomy, 234: 679-693.

612 Georgiou L., Kivell T.L., Pahr D.H., Skinner M.M. (2018) Trabecular bone patterning in the
613 hominoid distal femur. PeerJ, 6: e5156.

614 Goliath J.R., Ryan T.M., Gosman J.H. (2022) Ontogenetic patterning of human subchondral
615 bone microarchitecture in the proximal tibia. *Biology*: 11, 1-22.

616 Gray A.J., Villar R.N. (1997) The ligamentum teres of the hip: An arthroscopic classification
617 of its pathology. *Arthroscopy: The Journal of Arthroscopic & Related Surgery*, 13: 575-578.

618 Gross T., Kivell T.L., Skinner M.M. (2014) A CT-image-based framework for the holistic
619 analysis of cortical and trabecular bone morphology. *Palaeontol Electron*: 17, 13.

620 Guldberg R.E., Richards M., Caldwell N.J., Kuelske C.L., Goldstein S.A. (1997) Trabecular
621 bone adaptation to variations in porous-coated implant topology. *Journal of Biomechanics*,
622 30: 147-153.

623 Harrison L.C., Nikander R., Sikiö M., Luukkaala T., Helminen M.T., Ryymin P., Soimakallio
624 S., Eskola H.J., Dastidar P., Sievänen H. (2011) MRI texture analysis of femoral neck:
625 Detection of exercise load-associated differences in trabecular bone. *Journal of Magnetic
626 Resonance Imaging*, 34: 1359-1366.

627 Haxton H.A. (1947) Muscles of the pelvic limb. A study of the differences between bipeds and
628 quadrupeds. *The Anatomical Record*, 98: 337-346.

629 Hayama S. (1986) Spinal compensatory curvature found in Japanese macaques trained for the
630 acquisition of bipedalism. *Journal of Growth*, 25: 161-178.

631 Hayama S., Nakatsukasa M., Kunimatsu Y. (1992) Monkey performance: The development of
632 bipedalism in trained Japanese monkeys. *Acta anatomica Nipponica*, 67: 169-185.

633 Hayama S., Ogawa R., Sawada S., Okamoto T. (1985) The axial skeleton of Japanese
634 macaques in acquisition process of bipedalism by X-ray estimation. *Journal of the
635 Anthropological Society of Nippon*, 93: 223 (abstract).

636 Hayama S., Ueyama T., Ikeda M., Sakai T., Yamashita F., Yamamoto T., Arakawa H., Ogawa
637 R. (1986) The secondary curvature of the vertebral column of Japanese macaques in bipedal
638 acquisition process. *Acta anatomica Nipponica*, 61: 231 (abstract).

639 Higurashi Y., Goto R., Kumakura H. (2018) Intra-individual variation in hand postures during
640 terrestrial locomotion in Japanese macaques (*Macaca fuscata*). *Primates*, 59: 61-68.

641 Hirasaki E., Kumakura H., Matano S. (1993) Kinesiological characteristics of vertical climbing
642 in *Ateles geoffroyi* and *Macaca fuscata*. *Folia Primatologica*, 61: 148-156.

643 Hirasaki E., Ogihara N., Hamada Y., Kumakura H., Nakatsukasa M. (2004) Do highly trained
644 monkeys walk like humans? A kinematic study of bipedal locomotion in bipedally trained
645 Japanese macaques. *Journal of Human Evolution*, 46: 739-750.

646 Hirasaki E., Ogihara N., Hamada Y., Kumakura H., Nakatsukasa M. (2004) Do highly trained
647 monkeys walk like humans? A kinematic study of bipedal locomotion in bipedally trained
648 Japanese macaques. *Journal of human evolution*, 46: 739-750.

649 Hirasaki E., Ogihara N., Nakatsukasa M. (2006) Primates trained for bipedal locomotion as a
650 model for studying the evolution of bipedal locomotion. In: Ishida H., Tuttle R., Pickford
651 M., Ogihara N., Nakatsukasa M. (eds.), *Human Origins and Environmental Backgrounds*.
652 Springer, Boston, pp. 149-155.

653 Hoechel S., Schulz G., Müller-Gerbl M. (2015) Insight into the 3D-trabecular architecture of
654 the human patella. *Annals of Anatomy-Anatomischer Anzeiger*, 200: 98-104.

655 Hoemann C.D., Lafantaisie-Favreau C.H., Lascau-Coman V., Chen G., Guzman-Morales J.
656 (2012) The cartilage - bone interface. *Journal of Knee Surgery*, 25: 85-97.

657 Isler, K. (2005) 3D-Kinematics of vertical climbing in hominoids. *American Journal of Physical*
658 *Anthropology*, 126: 66-81.

659 Kapandji A.I. (2011) *The Physiology of the Joints*. Vol. 2. *The Lower Limb*, 6th ed. Elsevier,
660 Edinburgh.

661 Kaplan E.B. (1949) The ligamentum teres femoris in relation to the position of the femur.
662 *Bulletin of the Hospital for Joint Diseases*, 10: 112-117.

663 Kimura T. (1985) Bipedal and quadrupedal walking of primates: Comparative dynamics. In:
664 Kondo S. (ed.), Primate morphophysiology, locomotor analyses and human bipedalism.
665 University of Tokyo Press, Tokyo, pp. 81-104

666 Kimura T., Okada M., Ishida H. (1979) Kinesiological characteristics of primate walking: Its
667 significance in human walking. In: Morbeck M.E., Preushoft H., Comberg N. (eds.),
668 Environment, behavior, and morphology: Dynamic interactions in primates.

669 Kivell T.L. (2016) A review of trabecular bone functional adaptation: What have we learned
670 from trabecular analyses in extant hominoids and what can we apply to fossils? Journal of
671 Anatomy, 228: 569-594.

672 Kontulainen S., Sievänen H., Kannus P., Pasanen M., Vuori I. (2002) Effect of long-term
673 impact-loading on mass, size, and estimated strength of humerus and radius of female
674 racquetsports players: A peripheral quantitative computed tomography study between young
675 and old starters and controls. Journal of Bone and Mineral Research, 17: 2281-2289.

676 Lereim P., Goldie I., Dahlberg E. (1974) Hardness of the subchondral bone of the tibial
677 condyles in the normal state and in osteoarthritis and rheumatoid arthritis. Acta
678 Orthopaedica, 45: 614-627.

679 Lovejoy C.O. (2007) The natural history of human gait and posture: Part 3. The knee. Gait &
680 Posture, 25: 325-341.

681 Macchiarelli R., Nakatsukasa M., Rook L., Viola T.B., Bondioli L. (2001) Functional
682 adaptation of the iliac and the femoral cancellous network in a bipedal-trained Japanese
683 macaque. American Journal of Physical Anthropology, 32: 99 (abstract).

684 MacLatchy L., Müller R. (2002) A comparison of the femoral head and neck trabecular
685 architecture of *Galago* and *Perodicticus* using micro-computed tomography (ICT). Journal
686 of Human Evolution, 43: 89-105.

687 Mazurier A., Nakatsukasa M., Macchiarelli R. (2010) The inner structural variation of the
688 primate tibial plateau characterized by high-resolution microtomography. Implications for
689 the reconstruction of fossil locomotor behaviours. *Comptes Rendus Palevol*, 9: 349-359.

690 Mazurier A. (2006) Relations entre comportement locomoteur et variation cortico-trabéculaire
691 du plateau tibial chez les primates: analyse quantitative non invasive à haute résolution (SR-
692 - μ CT) et applications au registre fossile (Doctoral dissertation, Poitiers).

693 McKinley T.O., Bay B.K. (2001) Trabecular bone strain changes associated with cartilage
694 defects in the proximal and distal tibia. *Journal of Orthopaedic Research*, 19: 906-913.

695 Milz S., Putz R. (1994) Quantitative morphology of the subchondral plate of the tibial plateau.
696 *Journal of Anatomy*, 185: 103-110.

697 Mitra E., Rubin C., Qin Y.X. (2005) Interrelationship of trabecular mechanical and
698 microstructural properties in sheep trabecular bone. *Journal of Biomechanics*, 38: 1229-
699 1237.

700 Mori F., Tachibana A., Takasu C., Nakajima K., Mori S. (2001) Bipedal locomotion by the
701 normally quadrupedal Japanese monkey, *M. Fuscata*: Strategies for obstacle clearance and
702 recovery from stumbling. *Acta Physiologica et Pharmacologica Bulgarica*, 26: 147-150.

703 Mori S., Mori F., Nakajima K. (2006) Higher nervous control of quadrupedal vs bipedal
704 locomotion in non-human primates; Common and specific properties. In: Kimura H.,
705 Tsuchiya K., Ishiguro A., Witte H. (eds.), *Adaptive motion of animals and machines*.
706 Springer, Tokyo, pp. 53-65.

707 Mori S., Nakajima K., Mori F., Matsuyama K. (2004) Integration of multiple motor segments
708 for the elaboration of locomotion: Role of the fastigial nucleus of the cerebellum. *Progress*
709 *in Brain Research*, 143: 341-351.

710 Mulder B., Stock J.T., Saer J.P., Inskip S.A., Cessford C., Robb J.E. (2020) Intrapopulation
711 variation in lower limb trabecular architecture. *American Journal of Physical Anthropology*,
712 173: 112-129.

713 Murasaki Y. (1982) *Walk! Jump! Sampei*. Chikuma-shobo, Tokyo, p 247.

714 Murray A.A., Erlandson M.C. (2022) Tibial cortical and trabecular variables together can
715 pinpoint the timing of impact loading relative to menarche in premenopausal females.
716 *American Journal of Human Biology*, 34: e23711.

717 Nakajima K., Mori F., Takasu C., Mori M., Matsuyama K., Mori S. (2004) Biomechanical
718 constraints in hindlimb joints during the quadrupedal versus bipedal locomotion of *M.*
719 *fuscata*. *Progress in Brain Research*, 143: 183-190.

720 Nakano Y., Ishida H., Hirasaki E. (1996) The change of the locomotor pattern caused by the
721 inclination of the substrata in a Japanese macaque. *Primate Research*, 12: 79-87.

722 Nakano Y. (1996) Footfall patterns in the early development of the quadrupedal walking of
723 Japanese macaques. *Folia Primatologica*, 66: 113-125.

724 Nakatsukasa M., Hayama S. (2003) Skeletal response to bipedalism in macaques: With
725 emphasis on cortical bone distribution of the femur. *Cour Forschungsinst Senckenberg*, 243:
726 35-45.

727 Nakatsukasa M. (2004) Acquisition of bipedalism: The Miocene hominoid record and modern
728 analogues for bipedal protohominids. *Journal of Anatomy*, 204: 385-402.

729 Nakatsukasa M., Hayama S., Preuschoft H. (1995) Postcranial skeleton of a macaque trained
730 for bipedal standing and walking and implications for functional adaptation. *Folia Primatol*,
731 64: 1-29.

732 Nakatsukasa M., Hirasaki E., Ogiwara N. (2006) Energy expenditure of bipedal walking is
733 higher than that of quadrupedal walking in Japanese macaques. *American Journal of*
734 *Physical Anthropology*, 131: 33-37

735 Negayama K. (1983) Development of locomotor behavior in infant Japanese macaques
736 (*Macaca fuscata*). *Annales des Sciences Naturelles: Zoologie*, 5: 169-180.

737 O'Donnell J.M., Arora M. (2018) A novel and simple classification for ligamentum teres
738 pathology based on joint hypermobility. *Journal of Hip Preservation Surgery*, 5: 113-118.

739 O'Donnell J.M., Devitt B.M., Arora M. (2018) The role of the ligamentum teres in the adult
740 hip: Redundant or relevant? A review. *Journal of Hip Preservation Surgery*, 5: 15-22.

741 Odgaard A., Pedersen C.M., Bentzen S.M., Jorgensen J., Hvid I. (1989) Density changes at the
742 proximal tibia after meniscectomy. *Journal of Orthopaedic Research*, 7: 744-753.

743 Ogihara N., Hirasaki E., Andrada E., Blickhan R. (2018) Bipedal gait versatility in the Japanese
744 macaque (*Macaca fuscata*). *Journal of Human Evolution*, 125: 2-14.

745 Ogihara N., Hirasaki E., Kumakura H., Nakatsukasa M. (2007) Ground-reaction-force profiles
746 of bipedal walking in bipedally trained Japanese monkeys. *Journal of Human Evolution*, 53:
747 302-308.

748 Ogihara N., Makishima H., Aoi S., Sugimoto Y., Tsuchiya K., Nakatsukasa M. (2009)
749 Development of an anatomically based whole-body musculoskeletal model of the Japanese
750 macaque (*Macaca fuscata*). *American Journal of Physical Anthropology*, 139: 323-338.

751 Ogihara N., Makishima H., Nakatsukasa M. (2010) Three-dimensional musculoskeletal
752 kinematics during bipedal locomotion in the Japanese macaque, reconstructed based on an
753 anatomical model-matching method. *Journal of Human Evolution*, 58: 252-261.

754 Ogihara N., Usui H., Hirasaki E., Hamada Y., Nakatsukasa M. (2005) Kinematic analysis of
755 bipedal locomotion of a Japanese macaque that lost its forearms due to congenital
756 malformation. *Primates*, 46: 11-19.

757 Okada M. (1985) Primate bipedal walking: Comparative kinematics. In: Kondo S (ed.), *Primate*
758 *Morphophysiology, Locomotor Analysis, and Human Bipedalism*. University of Tokyo
759 Press, Tokyo, pp 47-58.

760 Pahr D.H., Zysset P.K. (2009). A comparison of enhanced continuum FE with micro FE models
761 of human vertebral bodies. *Journal of Biomechanics*, 42: 455-462.

762 Pearson O.M., Lieberman D.E. (2004) The aging of Wolff's "law": Ontogeny and responses
763 to mechanical loading in cortical bone. *The Yearbook of Physical Anthropology*, 47: 63-99.

764 Philippon M.J., Rasmussen M.T., Turnbull T.L., Trindade C.A., Hamming M.G., Ellman M.B.,
765 Wijdicks C.A. (2014) Structural properties of the native ligamentum teres. *Orthopaedic*
766 *Journal of Sports Medicine*, 2: 2325967114561962.

767 Polk J.D., Blumenfeld J., Ahluwalia D. (2008) Knee posture predicted from subchondral
768 apparent density in the distal femur: An experimental validation. *Anatomical Record*, 291:
769 293-302.

770 Pontzer H., Lieberman D.E., Momin E., Devlin M.J., Polk J.D., Hallgrímsson B., Cooper D.
771 M.L. (2006) Trabecular bone in the bird knee responds with high sensitivity to changes in
772 load orientation. *The Journal of Experimental Biology*, 209: 57-65.

773 Preuschoft H., Hayama S., Günther M.M. (1988) Curvature of the lumbar spine as a
774 consequence of mechanical necessities in Japanese macaques trained for bipedalism. *Folia*
775 *Primatologica*, 50: 42-58.

776 Profico A., Bondioli L., Raia P., O'Higgins P., Marchi D. (2021) Morphomap: An R package
777 for long bone landmarking, cortical thickness, and cross-sectional geometry mapping.
778 *American Journal of Physical Anthropology*, 174: 129-139.

779 Puymerail, L. (2011) Caractérisation de l'endostructure et des propriétés biomécaniques de la
780 diaphyse fémorale: la signature de la bipédie et la reconstruction des paléo-répertoires
781 posturaux et locomoteurs des hominines. PhD Dissertation, Poitiers.

782 Raichlen D.A., Gordon A.D., Foster A.D., Webber J.T., Sukhdeo S.M., Scott R.S., Gosman
783 J.H., Ryan T.M. (2015) An ontogenetic framework linking locomotion and trabecular bone

784 architecture with applications for reconstructing hominin life history. *Journal of Human*
785 *Evolution*, 81: 1-12.

786 Rao J., Zhou Y.X., Villar R.N. (2001) Injury to the ligamentum teres: Mechanism, findings,
787 and results of treatment. *Clinics in Sports Medicine*, 20: 791-800.

788 Renault J.B., Carmona M., Tzioupis C., Ollivier M., Argenson J.N., Parratte S., Chabrand P.
789 (2020) Tibial subchondral trabecular bone micromechanical and microarchitectural
790 properties are affected by alignment and osteoarthritis stage. *Scientific reports*, 10: 1-10.

791 Richmond B.G., Nakatsukasa M., Griffin N.L., Ogihara N., Ketcham R.A. (2005) Trabecular
792 bone structure in a bipedally-trained macaque. *American Journal of Physical Anthropology*,
793 40:175-176 (abstract).

794 Ritter M.A., Davis K.E., Small S.R., Merchun J.G., Farris A. (2014) Trabecular bone density
795 of the proximal tibia as it relates to failure of a total knee replacement. *The Bone & Joint*
796 *Journal*, 96: 1503-1509.

797 Roberts B.C., Solomon L.B., Mercer G., Reynolds K.J., Thewlis D., Perilli, E. (2017) Joint
798 loading and proximal tibia subchondral trabecular bone microarchitecture differ with
799 walking gait patterns in end-stage knee osteoarthritis. *Osteoarthritis and Cartilage*, 25: 1623-
800 1632.

801 Robling A.G., Hinant F.M., Burr D.B., Turner C.H. (2002) Improved bone structure and
802 strength after long-term mechanical loading is greatest if loading is separated into short
803 bouts. *Journal of Bone and Mineral Research*, 17: 1545-1554.

804 Ruff C.B., Holt B., Trinkaus E. (2006) Who's afraid of the big bad Wolff? "Wolff's law" and
805 bone functional adaptation. *American Journal of Physical Anthropology*, 129: 484-498.

806 Ryan T.M., Carlson K.J., Gordon A.D., Jablonski N., Shaw C.N., Stock J.T. (2018) Human-
807 like hip joint loading in *Australopithecus africanus* and *Paranthropus robustus*. *Journal of*
808 *Human Evolution*, 121: 12-24.

809 Ryan T.M., Ketcham R.A. (2002a) The three-dimensional structure of trabecular bone in the
810 femoral head of strepsirrhine primates. *Journal of Human Evolution*, 43: 1-26.

811 Ryan T.M., Ketcham R.A. (2002b) Femoral head trabecular bone structure in two omomyid
812 primates. *Journal of Human Evolution*, 43: 241-263.

813 Ryan T.M., Ketcham R.A. (2005) Angular orientation of trabecular bone in the femoral head
814 and its relationship to hip joint loads in leaping primates. *Journal of Morphology*, 265: 249-
815 263.

816 Ryan T.M., Krovitz G.E. (2006) Trabecular bone ontogeny in the human proximal femur.
817 *Journal of Human Evolution*, 51: 591-602.

818 Ryan T.M., Shaw C.N. (2012) Unique suites of trabecular bone features characterize locomotor
819 behavior in human and non-human anthropoid primates. *PLoS One*, 7: 1-11.

820 Ryan T.M., Shaw C.N. (2015) Gracility of the modern *Homo sapiens* skeleton is the result of
821 decreased biomechanical loading. *Proceedings of the National Academy of Sciences*, 112:
822 372-377.

823 Ryan T.M., Shaw C.N. (2015) Gracility of the modern *Homo sapiens* skeleton is the result of
824 decreased biomechanical loading. *Proceedings of the National Academy of Sciences*, 112:
825 372-377.

826 Ryan T.M., Walker A. (2010) Trabecular bone structure in the humeral and femoral heads of
827 anthropoid primates. *Anatomical Record*, 293: 719-729.

828 Saers J.P., Gordon A.D., Ryan T.M., Stock J.T. (2022) Growth and development of trabecular
829 structure in the calcaneus of Japanese macaques (*Macaca fuscata*) reflects locomotor
830 behavior, life history, and neuromuscular development. *Journal of Anatomy*, 241: 67-81.

831 Saers J.P.P., Cazorla-Bak Y., Shaw C.N., Stock J.T., Ryan T.M. (2016) Trabecular bone
832 structural variation throughout the human lower limb. *Journal of Human Evolution*, 97: 97-
833 108.

834 Saers J.P.P., DeMars L.J., Stephens N.B., Jashashvili T., Carlson K.J., Gordon A.D., Shaw C.N.,
835 Ryan T.M., Stock J.T. (2021) Combinations of trabecular and cortical bone properties
836 distinguish various loading modalities between athletes and controls. *American Journal of*
837 *Physical Anthropology*, 174: 434-450.

838 Saporin P., Scherf H., Hublin J.-J., Fratzl P., Weinkamer R. (2011) Structural adaptation of
839 trabecular bone revealed by position resolved analysis of proximal femora of different
840 primates. *Anatomical Record*, 294: 55-67.

841 Shaw C.N., Ryan T.M. (2012) Does skeletal anatomy reflect adaptation to locomotor patterns?
842 Cortical and trabecular architecture in human and nonhuman anthropoids. *American Journal*
843 *of Physical Anthropology*, 147: 187-200.

844 Skerry T.M., Lanyon L.E. (1995) Interruption of disuse by short duration walking exercise does
845 not prevent bone loss in the sheep calcaneus. *Bone*, 16: 269-274.

846 Stock J.T. (2006) Hunter-gatherer postcranial robusticity relative to patterns of mobility,
847 climatic adaptation, and selection for tissue economy. *American Journal of Physical*
848 *Anthropology*, 131: 194-204.

849 Su A., Carlson K.J. (2017) Comparative analysis of trabecular bone structure and orientation in
850 South African hominin tali. *Journal of Human Evolution*, 106: 1-18.

851 Sukhdeo S., Parsons J., Niu X.M., Ryan T.M. (2020) Trabecular bone structure in the distal
852 femur of humans, apes, and baboons. *Anatomical Record*, 303: 129-149.

853 Sylvester A.D., Terhune C.E. (2017) Trabecular mapping: Leveraging geometric
854 morphometrics for analyses of trabecular structure. *American Journal of Physical*
855 *Anthropology*, 163: 553-569.

856 Synek A., Dunmore C.J., Kivell T L., Skinner M.M., Pahr D.H. (2019) Inverse remodelling
857 algorithm identifies habitual manual activities of primates based on metacarpal bone
858 architecture. *Biomechanics and Modeling in Mechanobiology*, 18: 399-410.

859 Tardieu C. (1983) L'articulation du genou: analyse morpho-fonctionnelle chez les primates et
860 les hominidés fossiles. FeniXX.

861 Tsegai Z.J., Kivell T.L., Gross T., Nguyen N.H., Pahr D.H., Smaers J.B., Skinner M.M. (2013)
862 Trabecular bone structure correlates with hand posture and use in hominoids. PLoS One, 8:
863 e78781.

864 Tsegai Z.J., Skinner M.M., Pahr D.H., Hublin J.J., Kivell T.L. (2018) Systemic patterns of
865 trabecular bone across the human and chimpanzee skeleton. Journal of Anatomy, 232: 641-
866 656.

867 van Arkel R.J., Amis A.A., Cobb J.P., Jeffers J.R.T. (2015) The capsular ligaments provide
868 more hip rotational restraint than the acetabular labrum and the ligamentum teres: An
869 experimental study. The Bone & Joint Journal, 97: 484-491.

870 Veneziano A., Cazenave M., Alfieri F., Panetta D., Marchi, D. (2021) Novel strategies for the
871 characterization of cancellous bone morphology: Virtual isolation and analysis. American
872 Journal of Physical Anthropology, 175: 920-930.

873 Villar R.N., Santori N. (2012) In: Bird J.W.T. (ed), Operative Hip Arthroscopy. 3rd Ed.
874 Springer-Verlag, New York, pp. 117-128.

875 Volpato V., Viola T.B., Nakatsukasa M., Bondioli L., Macchiarelli R. (2007) Textural
876 characteristics of the iliac-femoral trabecular pattern in a bipedally trained Japanese
877 macaque. Primates, 49: 16-25.

878 Weatherholt A.M., Fuchs R.K., Warden S.J. (2013) Cortical and trabecular bone adaptation to
879 incremental load magnitudes using the mouse tibial axial compression loading model. Bone,
880 52: 372-379.

881 Wickham H. (2009) ggplot2: Elegant Graphics for Data Analysis. Springer-Verlag, New York.

882 **Captions to figures**

883 Figure 1. The upper rows represent the virtual morphometric maps, in medial view, of all
884 trabecular bone volume (BV/TV, %), trabecular thickness (Tb.Th., mm), degree of anisotropy
885 (DA) and trabecular spacing (Tb.Sp., mm) values in the femoral heads (only subchondral layer
886 is therefore visible) of the bipedally-trained macaque *Sansuke* and in the right femur of a wild
887 *Macaca fuscata* (KAS 266). The lower rows represent the deeper portion of the femoral head
888 of the values higher than 80% of the range of variation for the BV/TV, Tb.Th, and DA and the
889 values lower than 20% of the range of variation for the Tb.Sp. For each individual, chromatic
890 scale ranges from the minimum value (blue) to the maximum value (red). The left femur of
891 *Sansuke* has been mirrored as a right femur.

892

893 Figure 2. Box- and violin plots of relative bone volume (BV/TV), trabecular thickness
894 (Tb.Th.), trabecular spacing (Tb.Sp.) and degree of anisotropy (DA) of the femoral head of the
895 study sample. Values are standardized by the mean for each individual. Violin plots show the
896 kernel density distribution (including the minimum and maximum values) while the box and
897 whisker plots show the median and quartiles.

898

899 Figure 3. The upper rows represent the virtual morphometric maps, in medial view, of all
900 trabecular bone volume (BV/TV, %), trabecular thickness (Tb.Th., mm), degree of anisotropy
901 (DA) and trabecular spacing (Tb.Sp., mm) values in the proximal tibiae (only subchondral layer
902 is therefore visible) of the bipedally-trained macaque *Sansuke* and in the right proximal tibia of
903 a wild *Macaca fuscata* (KAS 266). The lower rows represent the deeper portion of the proximal
904 tibia of the values higher than 80% of the range of variation for the BV/TV, Tb.Th, and DA and
905 the values lower than 20% of the range of variation for the Tb.Sp. For each individual,
906 chromatic scale ranges from the minimum value (blue) to the maximum value (red). The left
907 tibia of *Sansuke* has been mirrored as a right tibia.

908

909 Figure 4. Box- and violin plots of relative bone volume (BV/TV), trabecular thickness
910 (Tb.Th.), trabecular spacing (Tb.Sp.) and degree of anisotropy (DA) of the proximal tibia of the
911 study sample. Values are standardized by the mean for each individual. Violin plots show the
912 kernel density distribution (including the minimum and maximum values) while the box and
913 whisker plots show the median and quartiles.

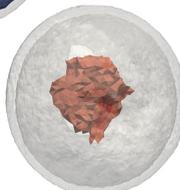
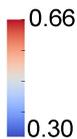
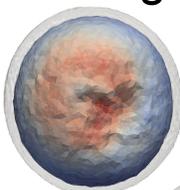
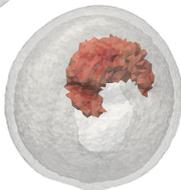
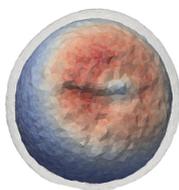
914

Sansuke
left

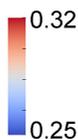
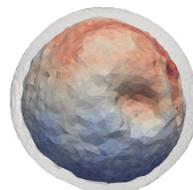
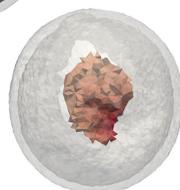
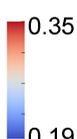
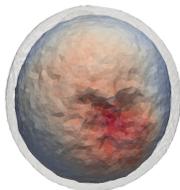
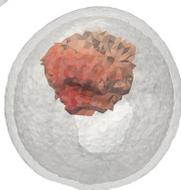
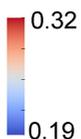
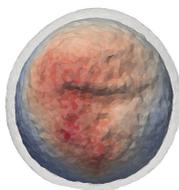
Sansuke
right

KAS 266

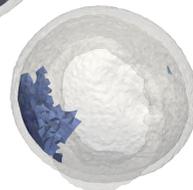
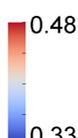
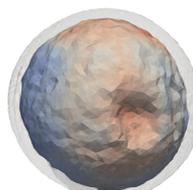
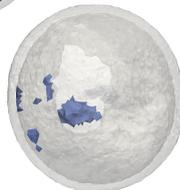
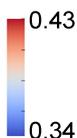
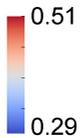
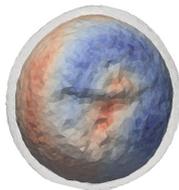
BV/TV



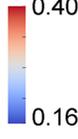
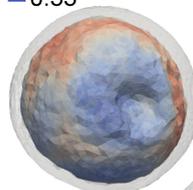
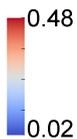
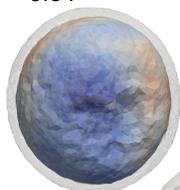
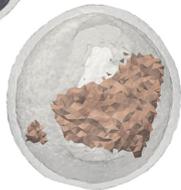
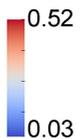
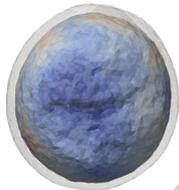
Tb.Th.



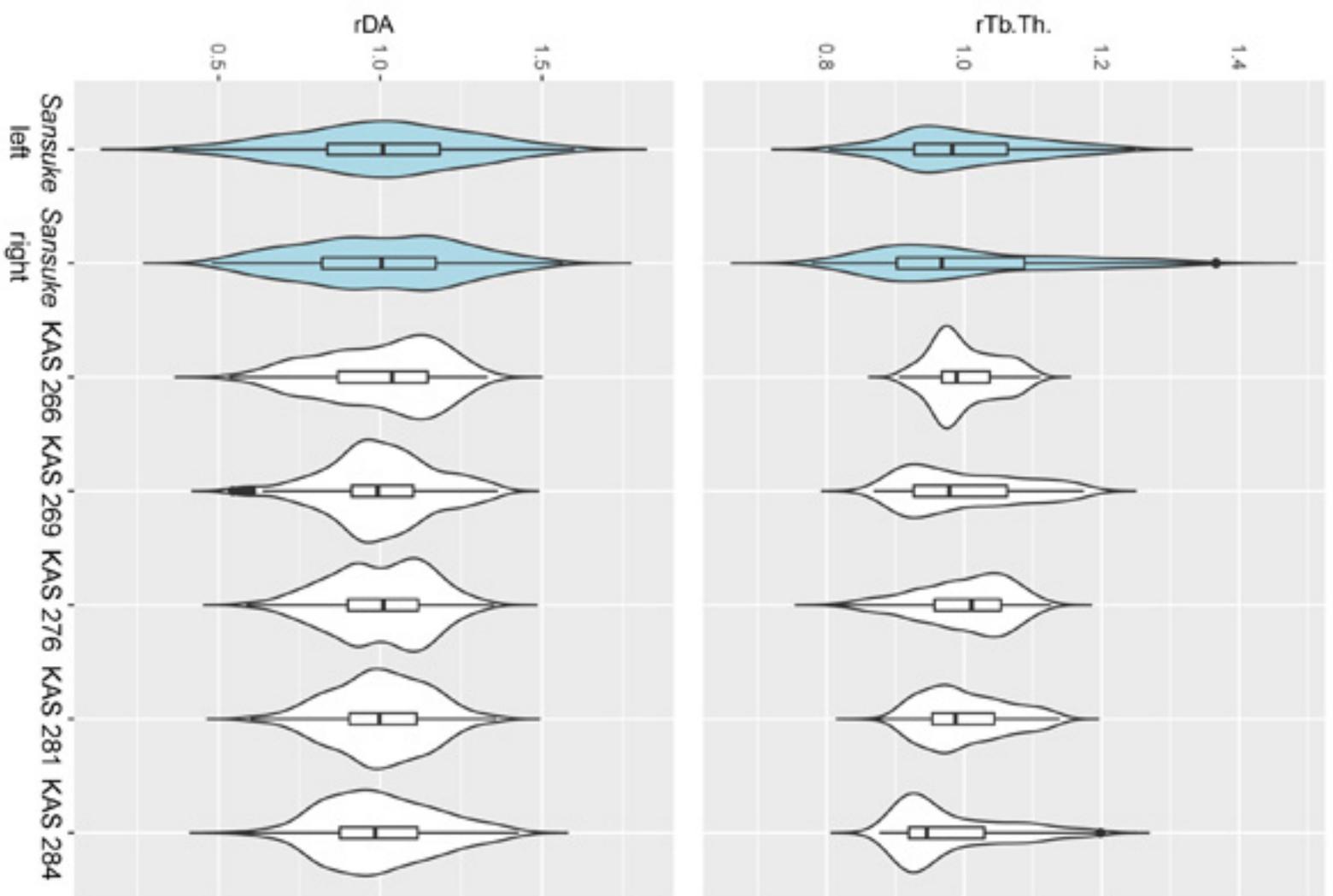
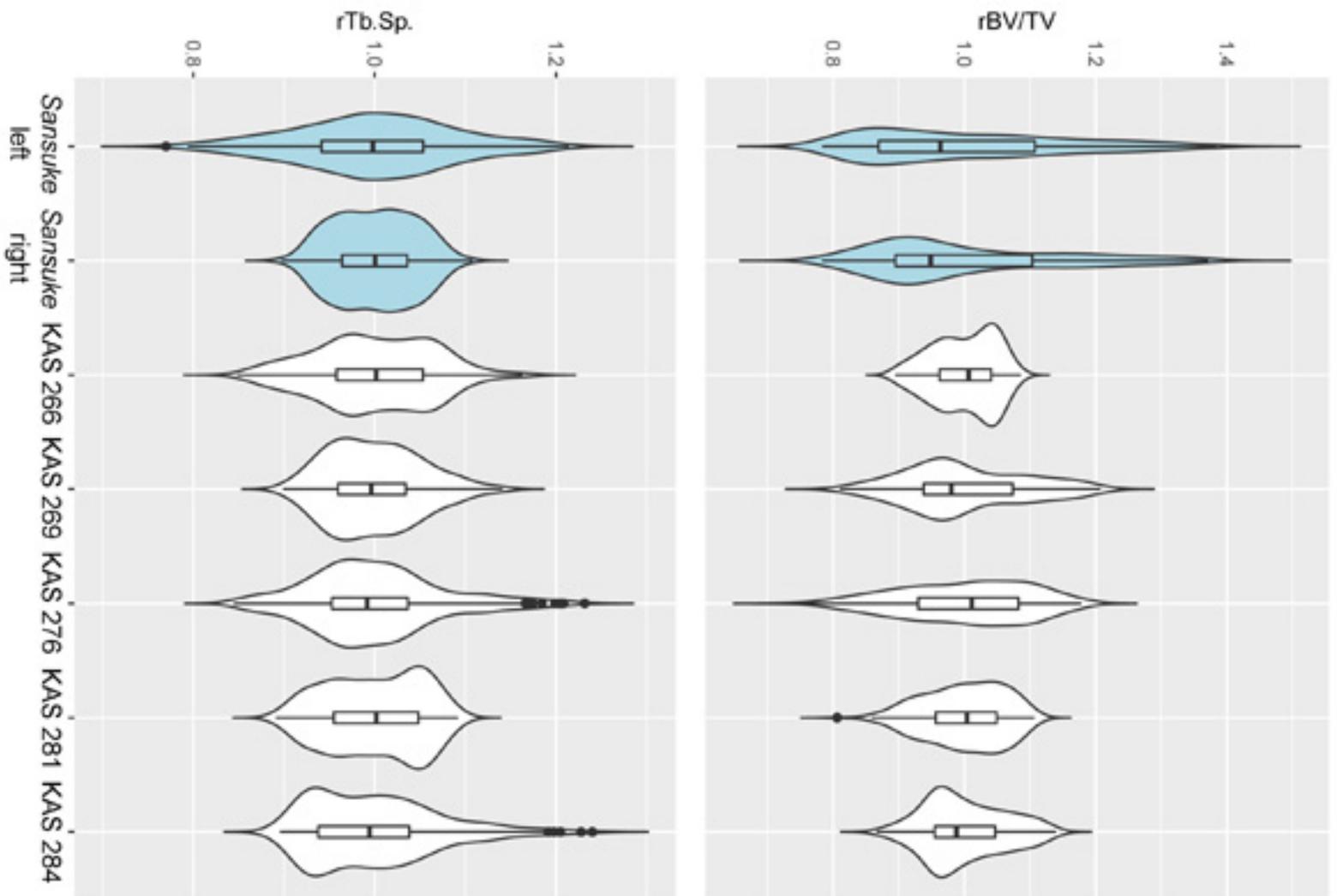
Tb.Sp.



DA



ant.
inf.

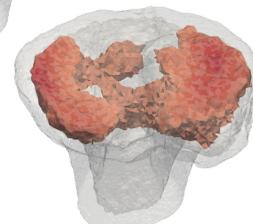
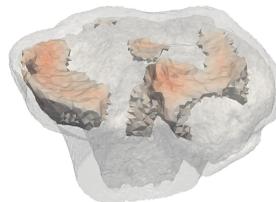
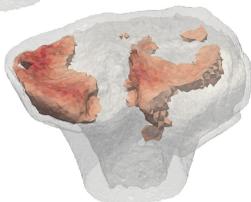
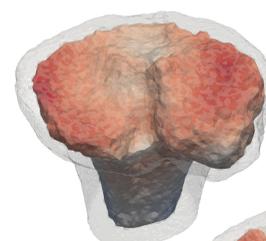
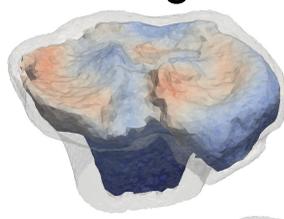
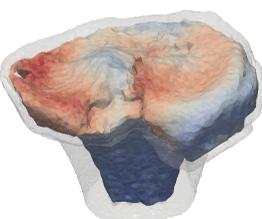


Sansuke
left

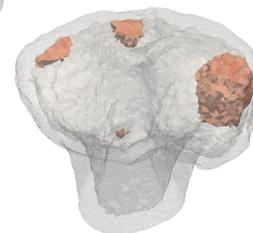
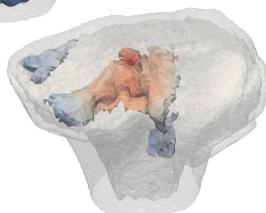
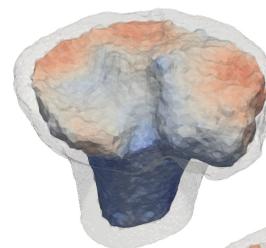
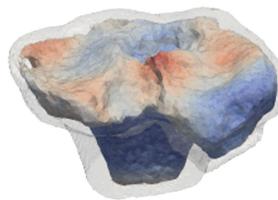
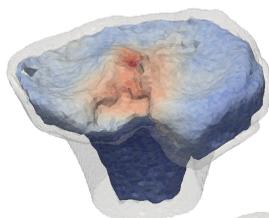
Sansuke
right

KAS 266

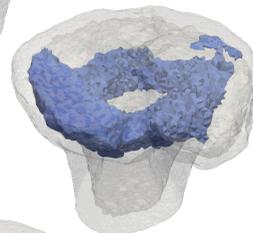
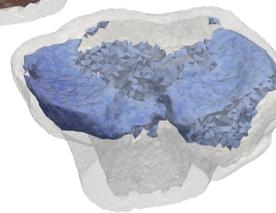
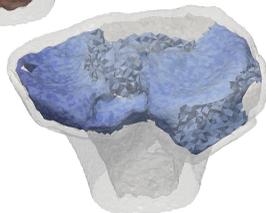
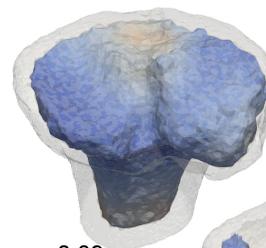
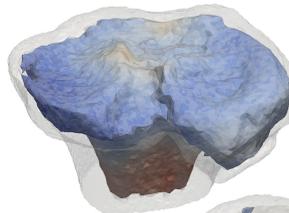
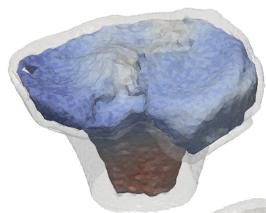
BV/TV



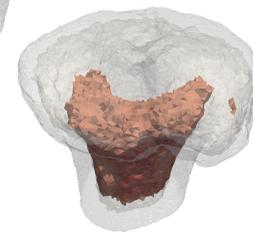
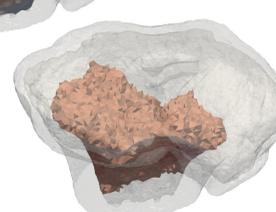
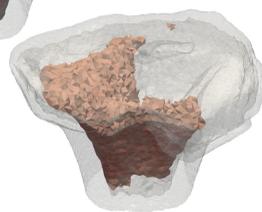
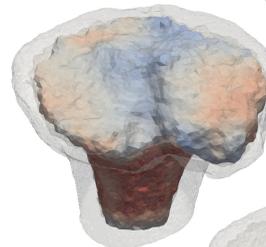
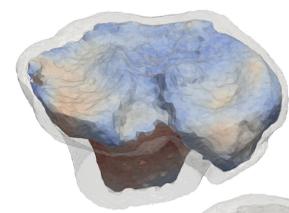
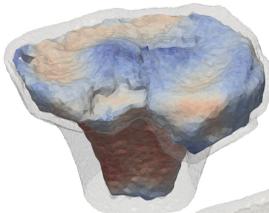
Tb.Th.



Tb.Sp.



DA



prox.
lat.

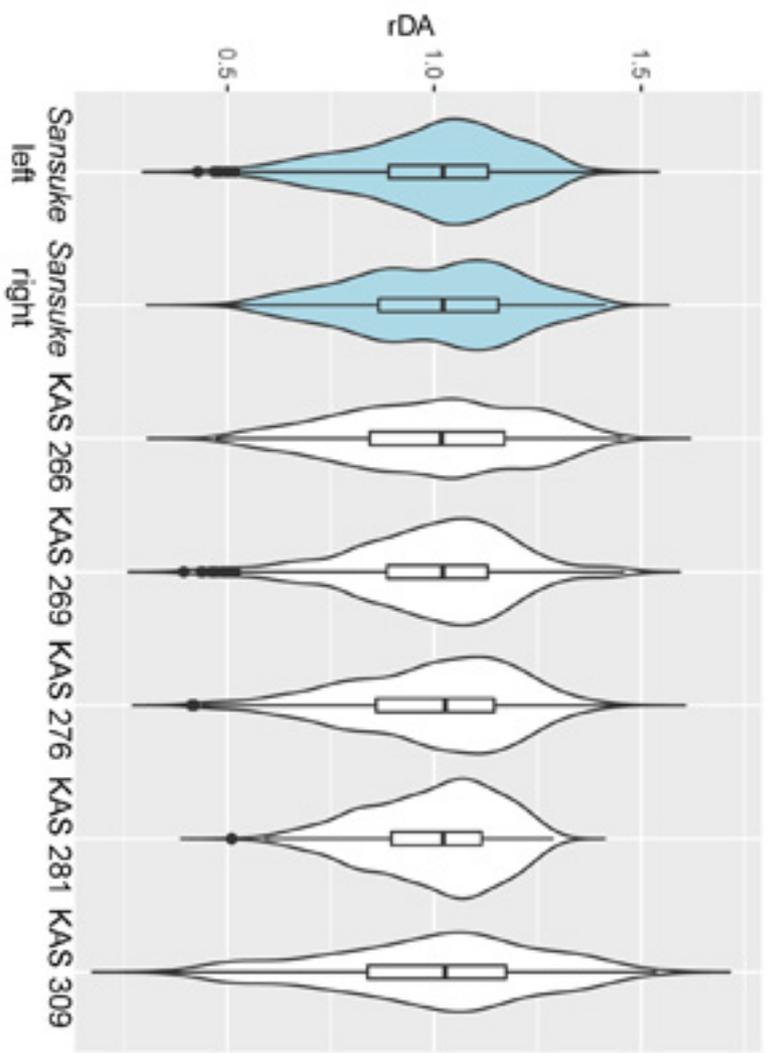
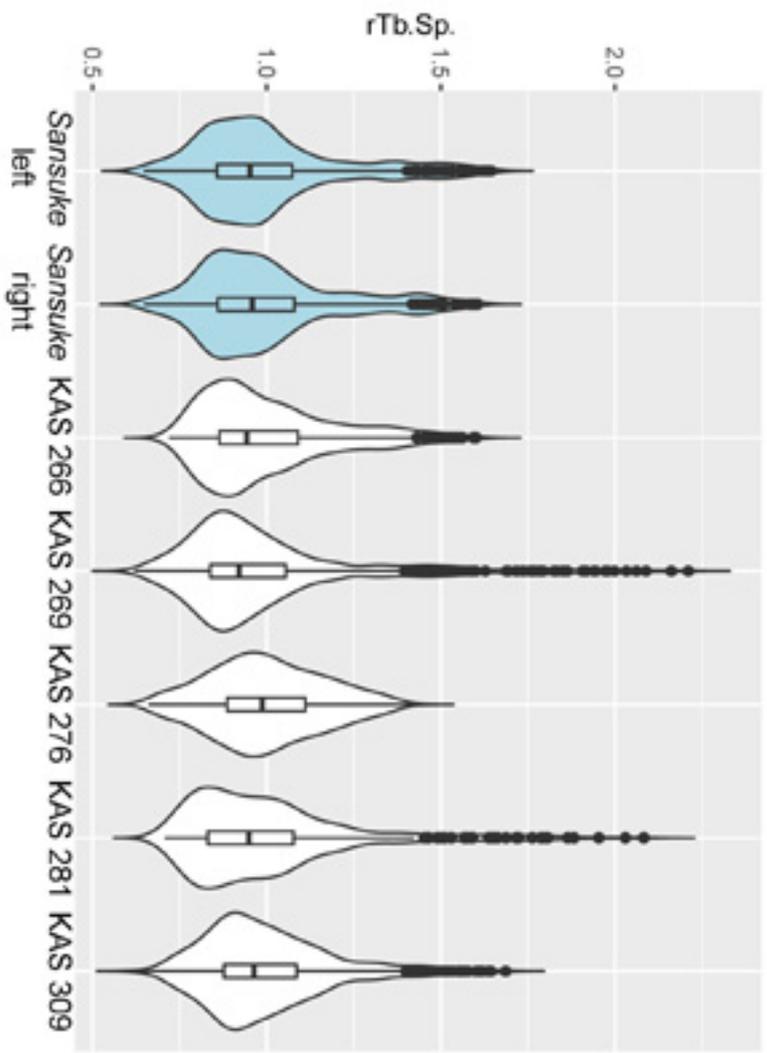
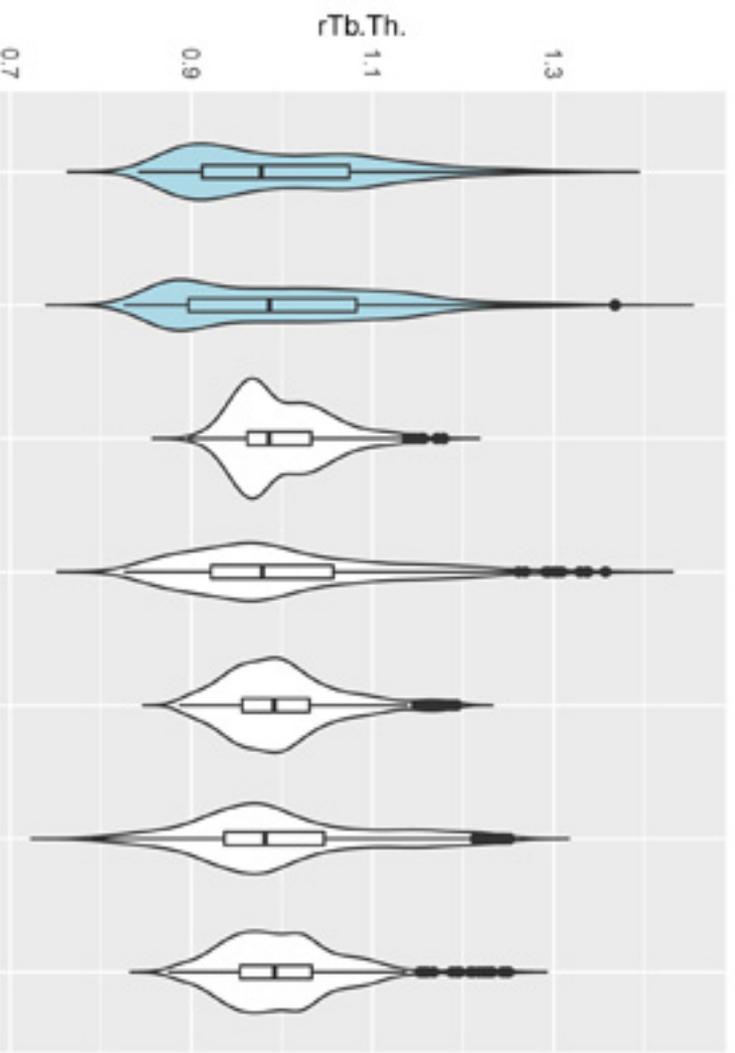
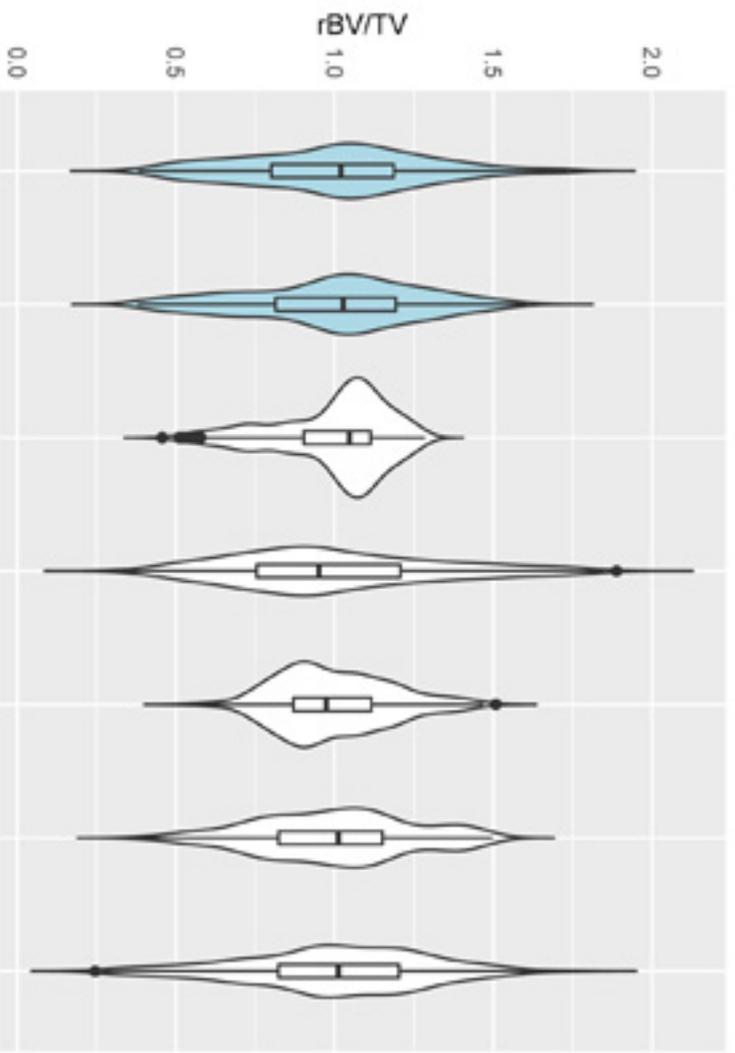


Table 1. Results of the Pearson's correlation tests between the trabecular bone density (BV/TV), trabecular thickness (Tb.Th.), trabecular spacing (Tb.Sp.) and degree of anisotropy (DA) of the femoral head calculated for the left and right proximal femora of the bipedally-trained macaque *Sansuke* and for the right femora of five wild *Macaca fuscata*. Strong correlations ($r > 0.8$) are in bold; significant correlations (p -value < 0.05) are noted with an asterisk.

Specimens	Parameters	BV/TV	Tb.Th.	Tb.Sp.
<i>Sansuke</i> left	Tb.Th.	0.96*	-	-
	Tb.Sp.	-0.13*	0.10	-
	DA	-0.76*	-0.83*	-0.04
<i>Sansuke</i> right	Tb.Th.	0.90*	-	-
	Tb.Sp.	-0.58*	-0.26*	-
	DA	-0.77*	-0.71*	0.35*
KAS 266	Tb.Th.	0.63*	-	-
	Tb.Sp.	-0.38*	0.45*	-
	DA	0.54*	0.35*	-0.34*
KAS 269	Tb.Th.	0.88*	-	-
	Tb.Sp.	-0.44*	0.00	-
	DA	0.04	-0.19*	-0.58*
KAS 276	Tb.Th.	0.61*	-	-
	Tb.Sp.	-0.44*	0.36*	-
	DA	-0.32*	-0.21*	-0.07
KAS 281	Tb.Th.	0.76*	-	-
	Tb.Sp.	-0.30*	0.37*	-
	DA	0.10	-0.14*	-0.47*
KAS 284	Tb.Th.	0.76*	-	-
	Tb.Sp.	-0.10	0.45*	-
	DA	-0.09	-0.45*	-0.49*

Table 2. Results of the Pearson's correlation tests between the trabecular bone density (BV/TV), trabecular thickness (Tb.Th.), trabecular spacing (Tb.Sp.) and degree of anisotropy (DA) of the proximal tibia calculated for the left and right tibiae of the bipedally-trained macaque *Sansuke* and for the right tibiae of five wild *Macaca fuscata*. Strong correlations ($r > 0.8$) are in bold; significant correlations (p -value < 0.05) are noted with an asterisk.

Specimens	Parameters	BV/TV	Tb.Th.	Tb.Sp.
<i>Sansuke</i> left	Tb.Th.	0.74*	-	-
	Tb.Sp.	-0.89*	-0.41*	-
	DA	-0.39*	-0.69*	0.20*
<i>Sansuke</i> right	Tb.Th.	0.81*	-	-
	Tb.Sp.	-0.92*	-0.58*	-
	DA	-0.52*	-0.81*	0.32*
KAS 266	Tb.Th.	0.62*	-	-
	Tb.Sp.	-0.86*	-0.16*	-
	DA	-0.30*	-0.48*	-0.02
KAS 269	Tb.Th.	0.87*	-	-
	Tb.Sp.	-0.75*	-0.38*	-
	DA	0.22*	0.47*	0.10*
KAS 276	Tb.Th.	0.35*	-	-
	TbSp	-0.88*	-0.03	-
	DA	-0.12*	0.22*	-0.04
KAS 281	Tb.Th.	0.69*	-	-
	Tb.Sp.	-0.85*	-0.30*	-
	DA	0.15*	0.38*	-0.11*
KAS 309	Tb.Th.	0.79*	-	-
	Tb.Sp.	-0.89*	-0.54*	-
	DA	0.03	0.01	-0.16*

SUPPORTING INFORMATION

ANTHROPOLOGICAL SCIENCE

Identification of Functionally-Related Adaptations in the Trabecular Network of
the Proximal Femur and Tibia of a Bipedally-Trained Japanese Macaque

M. CAZENAVE^{1,2,3*}, M. NAKATSUKASA⁴, A. MAZURIER⁵, M. SKINNER²

¹Division of Anthropology, American Museum of Natural History, New York, New York, USA

²Skeletal Biology Research Centre, School of Anthropology and Conservation, University of Kent, Canterbury, UK

³Department of Anatomy, Faculty of Health Sciences, University of Pretoria, Pretoria, South Africa

⁴Laboratory of Physical Anthropology, Department of Zoology, Graduate School of Science, Kyoto University, Kyoto, Japan

⁵Institut de Chimie des Milieux et Matériaux de Poitiers (IC2MP), Université de Poitiers, UMR CNRS 7285, F-86073 Poitiers, France

*Correspondence to: Marine Cazenave, Division of Anthropology, American Museum of Natural History, New York, New York, USA

E-mail: marine.cazenave4@gmail.com

Table S1. Composition and microCT scanning information for the investigated sample of femora and tibiae of *Macaca fuscata*.

Specimen	Sex	Element	Side	Collection ^a	Scan location ^b	Voxel size (μm)
<i>Sansuke</i>	male	femur & tibia	left and right	PRI	ESRF	46x46x43
KAS 266	male	femur & tibia	right	PRI	LPA	42 & 55
KAS 269	male	femur & tibia	right	PRI	LPA	42 & 59
KAS 276	male	femur & tibia	right	PRI	ESRF	46x46x43
KAS 281	female	femur & tibia	right	PRI	LPA	42 & 59
KAS 284	male	femur	right	PRI	LPA	42
KAS 309	male	tibia	right	PRI	ESRF	46x46x43

^aPRI = Primate Research Institute of Kyoto University, Japan.

^bESRF = European Synchrotron Radiation Facility (medical beam line ID 17), Grenoble, France; LPA = Laboratory of Physical Anthropology, Kyoto University (ScanXmate A080s system), Japan.

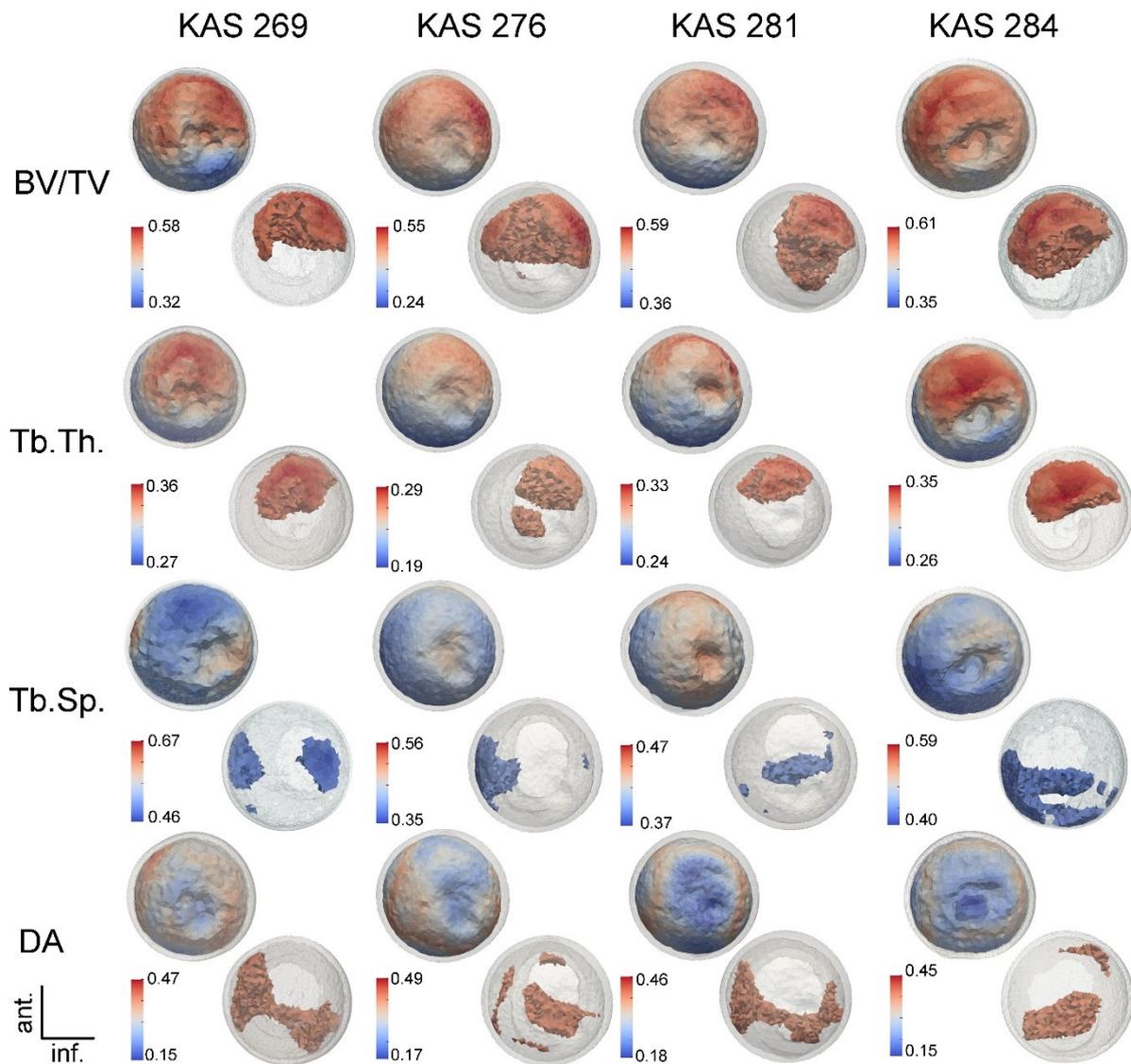


Figure S1. The upper rows represent the virtual morphometric maps, in medial view, of all trabecular bone volume (BV/TV, %), trabecular thickness (Tb.Th., mm), degree of anisotropy (DA) and trabecular spacing (Tb.Sp., mm) values in the femoral heads (only subchondral layer is therefore visible) in the right femur of wild *Macaca fuscata* (KAS 269, KAS 276, KAS 281, KAS 284). The lower rows represent the deeper portion of the femoral head of the values higher than 80% of the range of variation for the BV/TV, Tb.Th. and DA and the values lower than 20% of the range of variation for the Tb.Sp. For each individual chromatic scale ranging from the minimum value (blue) to the maximum value (red).

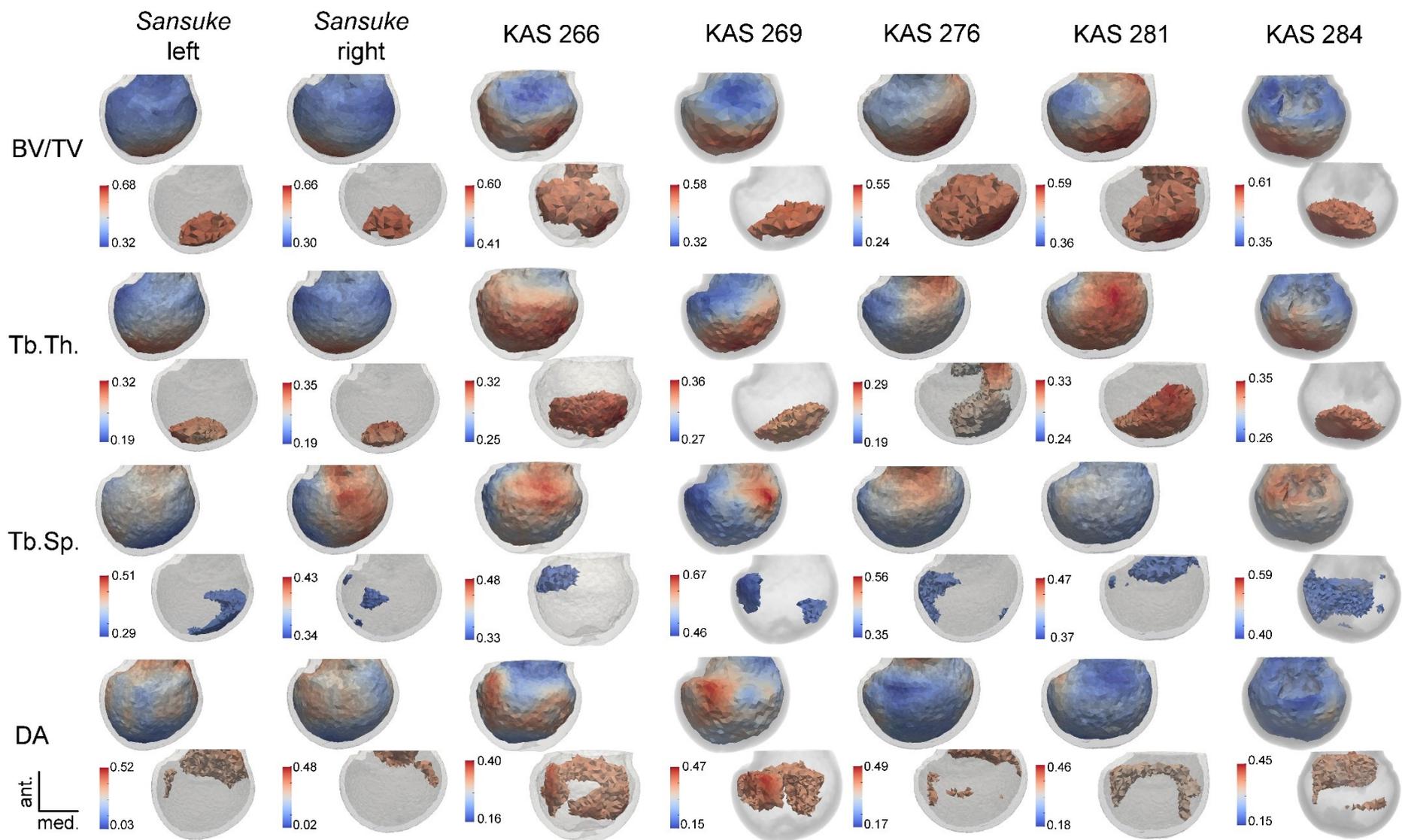


Figure S2. The upper rows represent the virtual morphometric maps, in superior view, of all trabecular bone volume (BV/TV, %), trabecular thickness (Tb.Th., mm), degree of anisotropy (DA) and trabecular spacing (Tb.Sp., mm) values in the femoral heads (only subchondral layer is therefore visible) in the left and right femora of the bipedally-trained macaque *Sansuke* and the right femur of wild *Macaca fuscata* (KAS 266, KAS 269, KAS 276, KAS 281, KAS 284). The lower rows represent the deeper portion of the femoral head of the values higher than 80% of the range of variation for the BV/TV, Tb.Th, and DA and the values lower than 20% of the range of variation for the Tb.Sp. For each individual chromatic scale ranging from the minimum value (blue) to the maximum value (red). The left femur of *Sansuke* has been mirrored as a right femur.

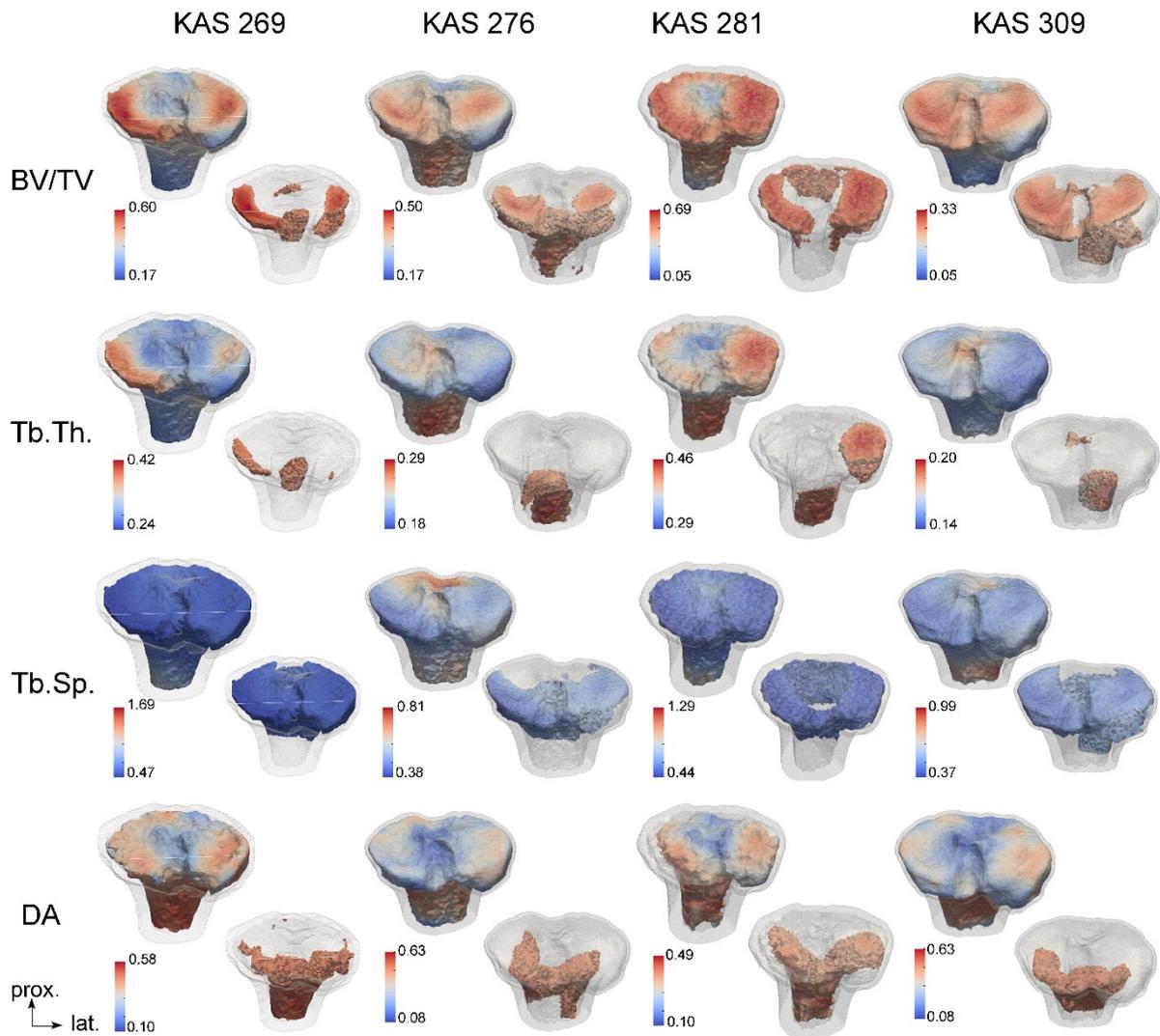


Figure S3. The upper rows represent the virtual morphometric maps, in medial view, of all trabecular bone volume (BV/TV, %), trabecular thickness (Tb.Th., mm), degree of anisotropy (DA) and trabecular spacing (Tb.Sp., mm) values in the proximal tibiae (only subchondral layer is therefore visible) in the right proximal tibia of a wild *Macaca fuscata* (KAS 269, KAS 276, KAS 281, KAS 309). The lower rows represent the deeper portion of the proximal tibia of the values higher than 80% of the range of variation for the BV/TV, Tb.Th., and DA and the values lower than 20% of the range of variation for the Tb.Sp. For each individual chromatic scale ranging from the minimum value (blue) to the maximum value (red).

