

1 Title: **Locating primary somatosensory cortex in human brain stimulation**  
2 **studies: Systematic review and meta-analytic evidence**

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4 Running head: Locating S1 in human brain stimulation studies

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15 Collected data, analysed data, wrote the paper: NPH

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17

18 **Abstract**

19 Transcranial magnetic stimulation (TMS) over human primary somatosensory cortex  
20 (S1), unlike over primary motor cortex (M1), does not produce an immediate,  
21 objective output. Researchers must therefore rely on one or more indirect methods to  
22 position the TMS coil over S1. The 'gold standard' method of TMS coil positioning is  
23 to use individual functional and structural magnetic resonance imaging (F/SMRI)  
24 alongside a stereotactic navigation system. In the absence of these facilities,  
25 however, one common method used to locate S1 is to find the scalp location which  
26 produces twitches in a hand muscle (e.g., the first dorsal interosseus, M1-FDI), then  
27 move the coil posteriorly to target S1. There has been no systematic assessment of  
28 whether this commonly-reported method of finding the hand area of S1 is optimal. To  
29 do this, we systematically reviewed 124 TMS studies targeting the S1 hand area, and  
30 95 functional magnetic resonance imaging (fMRI) studies involving passive finger  
31 and hand stimulation. 96 TMS studies reported the scalp location assumed to  
32 correspond to S1-hand, which was on average 1.5 to 2cm posterior to the  
33 functionally-defined M1-hand area. Using our own scalp measurements combined  
34 with similar data from MRI and TMS studies of M1-hand, we provide the estimated  
35 scalp locations targeted in these TMS studies of the S1-hand. We also provide a  
36 summary of reported S1 coordinates for passive finger and hand stimulation in fMRI  
37 studies. We conclude that S1-hand is more lateral to M1-hand than assumed by the  
38 majority of TMS studies.

39

40

41 **New and noteworthy**

42 Non-invasive methods of human brain stimulation involve applying electromagnetic  
43 stimuli to the scalp. To target a brain area, brain imaging or other measurement  
44 methods are used. Here, we systematically review the methods used to target  
45 transcranial magnetic stimulation onto the hand area of primary somatosensory  
46 cortex. We relate these targeted locations to our own scalp measurements and to a  
47 systematic review of functional magnetic resonance imaging data. We find that the  
48 most widely-used heuristic to locate the hand area of S1 is not optimal.

49

50 Keywords: S1, SI, TMS, TDCS, MRI

51 **1. Introduction**

52 In December 1908, the brain surgeon Harvey Cushing operated on the exposed  
53 postcentral gyrus of his patient, a 44 year old man who had recently developed  
54 epilepsy. Electrical stimulation to the cortex just posterior to the middle genu (now  
55 referred to as the 'hand knob', Yoursy et al. 1997) elicited sensations which the  
56 patient, wide awake and fully cooperative, described “*as though someone had*  
57 *touched or stroked the [right index] finger*” (Cushing 1909, p50).

58

59 More than a century after these remarkable and pioneering experiments, the  
60 localization of somatosensory function in the human cerebral cortex is still under  
61 study in neurosurgical patients (Hiremath et al. 2017). In non-clinical experiments  
62 with healthy participants, researchers can use non-invasive brain stimulation  
63 techniques such as transcranial magnetic stimulation (TMS, Barker et al. 1985) to  
64 study the human primary somatosensory cortex (S1).

65

66 S1 covers a large territory along the central sulcus and postcentral gyrus. While ‘S1  
67 proper’ is restricted to BA3b, we consider three distinct somatosensory cortical areas:  
68 BA3b, BA1, and BA2 (Geyer et al. 1999), collectively referring to them here as ‘S1’.  
69 Within S1 there are several topographically-organized maps of the body, representing  
70 the genitalia, feet, and legs medially, the upper arms superiorly, the forearms and  
71 hands laterally, and the face and internal organs laterally and ventrally. While the  
72 precise location of each body part representation, as well as the gross anatomy and  
73 folding of the pre- and postcentral sulci, may vary between people, the overall  
74 topography remains remarkably similar to the classic 'homunculus' as drawn by

75 Penfield and Boldrey (1937; Tamè et al. 2016). The topography in S1 is more finely-  
76 grained and more organized than that of neighboring M1 (Hlustik et al. 2001).

77

78 This within- and between-person consistency in the locations of different body part  
79 representations in S1 allows neuroscientists to aggregate and map the results from  
80 different people in studies of cortical somatosensory function. Functional magnetic  
81 resonance imaging (fMRI) data can, for example, provide reasonable estimates of  
82 the relative locations of body part representations in small samples of healthy  
83 participants, even when the data are transformed into the same, standard, coordinate  
84 frames (i.e., warping the shape and size of the brain image), and when averaging  
85 data over participants (Nelson and Chen, 2008). Likewise, studies using transcranial  
86 electrical, magnetic, or direct current stimulation (TES, TMS, TDCS) can rely on the  
87 topography of the neighboring primary motor cortex for stimulator placement over the  
88 'core region' of a given muscle (e.g., Weiss et al. 2013). Due to this reliable  
89 stimulation of the motor areas, along with clear, immediate and objective outputs in  
90 the form of stimulation-evoked body movement and muscle activity, good progress  
91 has been made in studying the human primary motor cortex in healthy participants  
92 (e.g., Raffin et al. 2015).

93

94 Progress has been slower, however, in understanding the electrical excitability of  
95 primary somatosensory cortex and its function in healthy participants. This is likely  
96 due, in part, to the lack of direct, immediate, and objective consequences of S1  
97 stimulation. While some early studies reported that TMS over M1 or S1 elicited  
98 'paraesthesias' or 'sensations of movement' in healthy participants (Amassian et al.

99 1991; Sugishita and Takayama, 1993), this phenomenon has not received systematic  
100 experimental attention (though see, e.g., Ragert et al. 2003; Tegenthoff et al. 2005,  
101 for anecdotal and pre-experimental evidence). The lack of immediate objective  
102 consequences following TMS over S1 means that researchers cannot be sure that  
103 the stimulating coil is correctly positioned, or that the stimulating current is sufficiently  
104 strong or properly oriented to activate the targeted neurons in S1. Reliable coil  
105 positioning is critical both to ensure stimulation of the correct brain area, but also to  
106 ensure adequate control of TMS-related side-effects (Meteyard & Holmes, 2018;  
107 Holmes & Meteyard, under review).

108

109 In previous work (Tamè & Holmes, 2016), we used individual fMRI neuronavigation  
110 to locate S1-hand in 20 healthy participants during a TMS study of tactile detection  
111 and discrimination. We noticed that, in every participant, the scalp location of S1-  
112 hand (specifically, the index and middle finger representations) was lateral to the  
113 scalp location of M1-hand (specifically, the first dorsal interosseus muscle  
114 representation, M1-FDI). This surprised us, as almost all the TMS literature that we  
115 were aware of had moved the TMS coil posteriorly to M1-FDI rather than laterally.  
116 Further, fMRI studies in which both M1 and S1 were measured in the same  
117 participants also showed that the S1 representation was lateral to the M1  
118 representation of the hand (Blatow et al. 2011).

119

120 The purpose of the present systematic review was therefore to summarize the  
121 available evidence concerning the location on the human scalp which researchers  
122 stimulate in TMS studies of S1, in particular the S1 representation of the hand and

123 fingers (S1-hand). We did this in several ways. First, we summarized all the available  
124 scalp measurements that we have collected during 35 previous TMS experiments  
125 conducted in our own laboratory. Specifically, we summarised those data pertaining  
126 to head size and the likely scalp coordinates overlying the representation of M1-FDI,  
127 which is often used as a reference-point for TMS studies of S1, along with the  
128 location of the C3/C4 electrode location in the 10:20 system (Jasper, 1954), another  
129 commonly-used reference. The purpose of systematically measuring the scalp in our  
130 prior work is to relate our TMS data to the 10:20 system, to measure between-  
131 participants variability in head size and shape, to provide informative prior estimates  
132 to assist future localizations, and to provide a check for measurement errors that may  
133 arise during neuronavigation. Second, we systematically reviewed the methods used  
134 to locate human S1-hand in previous TMS studies, focusing on the scalp locations  
135 targeted. Third, we reviewed previous attempts to relate positions on the scalp to the  
136 underlying positions in the brain. Finally, we systematically reviewed the brain  
137 locations activated following passive finger and hand stimulation in fMRI studies.  
138 These four components of the present work allowed us to relate the scalp locations  
139 stimulated in prior TMS studies of S1-hand, to the likely location of S1-hand in fMRI  
140 studies.

141

## 142 **Materials and methods**

143 All experimental studies received approval from local research ethics committees,  
144 and were conducted in accordance with international safety guidelines (Rossi et al.  
145 2009), and with the Declaration of Helsinki (2008 version, which does not require  
146 study pre-registration). Throughout the manuscript, we refer to scalp and brain

147 coordinates using the following convention: ORIGIN(lateral,anterior). For example,  
148 5cm left and 1cm anterior to the vertex origin, Cz, is written: Cz(-5,1), and 2cm  
149 posterior to the FDI muscle location is FDI(0,-2). Standard MNI neuroimaging  
150 coordinates are given as MNI(X,Y,Z), in mm. MRI data reported in Talairach and  
151 Tournoux (1988) coordinates were converted to MNI coordinates using Matthew  
152 Brett's tal2mni.m script implemented in several Matlab functions  
153 ([http://eeg.sourceforge.net/doc\\_m2html/bioelectromagnetism/mni2tal.html](http://eeg.sourceforge.net/doc_m2html/bioelectromagnetism/mni2tal.html)). All data  
154 and analysis scripts are available at <https://osf.io/c8nhj/>.

155

#### 156 *Head size and 10:20 locations*

157 The Hand Laboratory has been recording scalp locations during TMS experiments  
158 since 2012, and more thoroughly and systematically since 2016 (Protocol sheet  
159 available at <https://osf.io/c8nhj/>). Researchers measured the distance between  
160 nasion and inion, and between the pre-auricular points of the two ears. The  
161 intersection of these lines is marked as the vertex. For sites relatively close to the  
162 vertex and/or close to the pre-auricular axis (e.g., M1, S1), a rectangular coordinate  
163 frame (x-axis = right of vertex, y-axis = anterior to vertex) is suitable. For areas  
164 further away from vertex, this system would break down with the curvature of the  
165 skull, and a polar coordinate scheme is required. The lateral coordinate of a scalp  
166 location is always measured first, and the anterior coordinate second, measuring  
167 perpendicularly forwards or backwards from the vertex-preauricular line. The data are  
168 noted first on the protocol sheet, and transferred later to an electronic database  
169 (MySQL, accessed via custom web-based software ARM and LabMan,  
170 <https://github.com/TheHandLab>). As these scalp location data accumulate, they will



171 be made freely available via the TMS-SMART website (<http://tms-smart.info>). The  
172 HandLab database was queried for all available head measurements (N=284),  
173 aggregated by participant (N=101). Mean and SD within and between participants  
174 was calculated. The standard 10:20 system electrode locations C3/C4, often used in  
175 transcranial stimulation studies of S1-hand, were converted into distances measured  
176 along the scalp from the vertex by dividing the inter-preauricular distance by 5 (i.e.  
177 20%). Note that head size and shape is likely to vary widely across participants,  
178 probably more so than brain size and shape (Zilles et al. 2001; Xiao et al. 2018).

179

#### 180 *TMS over M1-FDI*

181 The HandLab database was queried for the mean scalp location stimulated during  
182 our TMS studies of primary motor cortex, specifically the contralateral representation  
183 of the FDI (N=127), aggregating the data by participant (N=65) and hemisphere.  
184 Measurements from the same participant were averaged prior to averaging across  
185 participants.

186

#### 187 *Systematic review of TMS over S1-index*

188 PubMed (<https://www.ncbi.nlm.nih.gov/pubmed/>) was searched with the query  
189 “(somatotop\* OR somatosens\* OR tact\* OR touch OR cutan\*) AND (TMS OR TDCS  
190 OR transcranial stimulation)” on 2<sup>nd</sup> January 2018, and again on 30<sup>th</sup> July 2018. The  
191 primary variables assessed were the methods used to locate the TMS coil over S1,  
192 including the body part targeted, anatomical reference points, coordinate system, and  
193 distances measured along the scalp or in the brain.

194

195 The reference sections of relevant articles were checked for additional articles, and  
196 citations between included articles were recorded. 1384 initial results were  
197 decreased to 299 (22%) potential articles on the basis of titles and abstracts. PDFs of  
198 291/299 (97%) were retrieved and inspected for relevant methods.

199

200 Inclusion criteria were experimental reports including TMS targeted over human S1.  
201 We restricted the analyses to TMS studies which either explicitly targeted the hand  
202 area of S1, used the hand area of M1 as a reference-point, or did not explicitly say  
203 which body part was targeted, but used the same methods as those studies which  
204 did target the hand area. For example, studies which positioned the TMS coil relative  
205 to a facial or foot muscle representation in M1 were excluded, but studies which  
206 positioned the TMS coil, for example over C3/C4, or over C3'/C4', or 2cm behind  
207 C3/C4, and which stated that this was over the 'somatosensory cortex' were included.

208

209 We excluded 12 review articles, 23 studies which targeted TMS over M1 or mapped  
210 M1, 48 studies which targeted other brain areas, 14 studies which did not report  
211 scalp coordinates, 41 studies which used other brain stimulation methods, 7 for other  
212 reasons, and 8 studies for which we could not access the full article. 14 additional  
213 studies from this search were excluded from the systematic review, but were relevant  
214 to the review of scalp-to-brain measurements, described below. 124/291 (43%)  
215 identified studies were included. 96/124 (77%) reported numerical coordinates for  
216 locating S1, met all other inclusion criteria, and are included in the analyses. We did  
217 not include or exclude studies based on the type of TMS equipment, experiment  
218 protocol, or participants tested – the purpose of the review was to identify the scalp

219 locations stimulated, not the effects of stimulation on the brain or somatosensory  
220 perception.

221

222 *Review of studies relating scalp and cortical anatomy*

223 During the systematic reviews, fourteen articles were found which provided methods  
224 of relating scalp locations for the EEG electrode locations C3/C4 or TMS over M1, to  
225 anatomical landmarks or coordinates. No systematic search or review was  
226 attempted, however the reference sections of these articles was searched and  
227 followed for additional potential articles.

228

229 *Systematic review of FMRI of S1-hand*

230 PubMed was searched with the query “(primary somatosensory cortex OR S1 OR SI)  
231 AND (FMRI OR functional magnetic resonance imaging) AND (hand OR finger OR  
232 digit)” on the 7<sup>st</sup> January, 2018, and again on 31<sup>st</sup> July, 2018. 1252 search results  
233 were combined with 28 additional articles found in the previous search. This was  
234 reduced to 389 (31%) potential articles on the basis of titles and abstracts, searching  
235 for any neuroimaging methods and any somatosensory stimuli. A second, more  
236 thorough, review checked abstracts and/or full papers for inclusion criteria, which  
237 were: a) used FMRI, b) reported atlas coordinates in a standardized space (Talairach  
238 and Tournoux, 1988, or Montreal Neurological Institute, MNI), c) tested healthy adult  
239 human participants, d) applied somatosensory stimulation to the digit(s) or hand(s),  
240 and e) reported activation in the central sulcus, post-central gyrus, and/or any part of  
241 S1, using a statistical contrast between passive stimulation and no stimulation.  
242 139/389 (36%) of studies were deemed relevant, but the full articles (.pdfs) were only

243 available for 95 (68%) of the relevant articles. Of the 293 excluded articles, 142  
244 (49%) did not report coordinates in 3 dimensions or reported coordinates only relative  
245 to other coordinates, 31 (11%) involved active hand movement, 30 (10%) did not use  
246 fMRI, 27 (9%) did not stimulate the hand, 25 (9%) contained data only from patients,  
247 children, or monkeys. The data from 4 further articles had been published elsewhere  
248 previously, 3 were purely anatomical studies, 3 were not in English, and 2 were not  
249 empirical studies. 26 (9%) were excluded because we could not access the full text.

250

251 The primary variable extracted from 95 selected articles was the reported 3D location  
252 of BOLD signal (peak voxel in group analysis, or mean across participants of peak  
253 voxel in individual analyses) in S1, including the body part targeted, the coordinate  
254 system used, and any anatomical or functional labels assigned to the coordinate.

255 Means and standard deviations (SD) across participants were recorded or calculated  
256 where individual data were available. Coordinates reported using the Talairach and  
257 Tournoux reference system (most often, studies using BrainVoyager software) were  
258 transformed into MNI space. During analysis, and following advice from reviewers,  
259 we further restricted the analysis to coordinates which were labeled as being in  
260 BA3b, BA1, or BA2, and which were within the 50% cytoarchitectural probability  
261 maps of these three areas. The on-line data and analysis scripts include additional  
262 variables not explored in the present work, including stimulus modality (i.e.,  
263 thermo/nociceptive, electrical, vibrotactile, brushing, and punctate stimulation).

264

265 *Limitations*

266 Due to limitations on time and resources, we did not use multiple independent

267 databases for the systematic reviews, and we did not use multiple independent  
268 coders to select articles from the 2,636 identified records or to extract the stimulation  
269 and activation data from the 219 included papers. For the TMS literature search, we  
270 tracked the citations of all articles identified in order to locate studies not found by the  
271 initial searches. This did not lead to any additional articles. We did not, therefore,  
272 repeat this search for the fMRI literature. Because we included all stimulus sub-  
273 modalities in our fMRI literature search, the resulting mean coordinates for S1-hand  
274 may not be sufficiently precise for future researchers interested in only one  
275 somatosensory sub-modality. To address these limitations, we have provided all our  
276 data and analysis scripts in supplementary on-line materials. We encourage other  
277 researchers to validate, extend, and improve our work, for example by implementing  
278 a more thorough literature search with multiple independent searchers (e.g.,  
279 Hayward et al. 2016), or by repeating the analyses using only their preferred sub-  
280 modality of stimulation.

281

## 282 *Analysis*

283 For all reported and measured scalp locations (lateral and anterior to the given  
284 reference point), and for reported fMRI coordinates (x, y, z), the means and standard  
285 deviations across studies were calculated, aggregating data across conditions where  
286 relevant. For fMRI studies which reported individual participants' coordinates, the  
287 mean across the individual coordinates was calculated within each study, separately  
288 for different brain areas (BA3b, BA1, BA2). Coordinates that were reported in  
289 Talairach (& Tournoux) space were converted into MNI space. Coordinates which  
290 were not reported as being in Talairach or MNI spaces were assigned to the most

291 likely space, according to the software used (e.g., MNI for SPM, Talairach for  
292 BrainVoyager), or else plot in 3D alongside all other MNI coordinates, both before  
293 and after applying the Talairach-to-MNI transform to identify the most likely space. If  
294 unsure, the data were assumed to be in MNI space. For calculation of 'weighted  
295 means' across studies, we multiplied the reported means by the reported number of  
296 participants, then divided the sum of these values across all studies by the grand  
297 total of all participants across all studies, to give a weighted mean location, either on  
298 the scalp or in MNI coordinates.

299

## 300 ***Results and statistical analyses***

### 301 ***Measurements of scalp size and 10:20 locations***

302 Across 101 participants, the mean $\pm$ SD head size was 35.9 $\pm$ 2.1cm (range: 31-41cm)  
303 from nasion toinion, and 35.9 $\pm$ 1.5cm (range: 33-40cm) between left and right pre-  
304 auricular points. This places the mean $\pm$ SD C3/C4 electrode sites, on average,  
305 7.2 $\pm$ 0.3cm (range: 6.6-7.8cm) lateral to the vertex (Figure 1). Forty-four participants'  
306 heads were measured more than once (range 2-23 measurements;  
307 mean $\pm$ SD=5.1 $\pm$ 4.7 measurements per participant). Of these, the head  
308 measurements varied within-participants and between-sessions, by as much as 5cm  
309 for nasion toinion (mean $\pm$ SD within-participants range=1.8 $\pm$ 1.4cm), and 4cm for pre-  
310 auricular distances (mean $\pm$ SD=1.3 $\pm$ 0.9cm). The large range of these measurements  
311 is likely due to human error.

312

### 313 ***TMS over M1-FDI***

314 *Across 108 measurements from 56 participants, the mean $\pm$ SD left hemisphere scalp*

315 *location of M1-FDI was  $5.2\pm0.8$ cm left of, and  $0.4\pm0.9$ cm anterior to the vertex*  
316 *(Figure 1). In 19 measurements from 14 participants, the mean $\pm$ SD right hemisphere*  
317 *M1-FDI location was  $5.2\pm0.9$ cm right of, and  $0.5\pm0.9$ cm anterior to the vertex.*

318

### 319 **Systematic review of TMS over S1-index**

320 TMS studies targeting S1-hand have used three main localization strategies. The first  
321 study (Cohen et al. 1991) applied the border of a round coil, or the center of a figure-  
322 of-eight coil over the C3/C4 electrode location. This method was followed by Seyal et  
323 al. (1992, 1993), Pascual-Leone and Torres (1993), Siebner et al. (1998) and Harris  
324 et al. (2002). Starting with Enomoto et al. (2001), other studies also used C3/C4 as a  
325 reference point, but moved the coil posteriorly by between 2 and 3.6cm. In total, 16  
326 studies used C3/C4 as a reference, and positioned the coil a mean $\pm$ SD of  $1.5\pm1.2$ cm  
327 posterior to C3/C4 (Table 1).

328

329 The second, and most common, strategy was to use the functionally-defined scalp  
330 location for a muscle in the hand (typically FDI, abductor pollicis brevis, APB, or  
331 opponens pollicis, OP) as a reference point. Starting with Sugishita and Takayama  
332 (1993), 43 such studies used MEPs to localize M1-FDI, then moved the coil  
333 posteriorly from that point on the scalp, by between 0 and 3cm  
334 (mean $\pm$ SD= $1.9\pm0.9$ cm). 16 additional studies used thenar muscles (APB, OP) to  
335 locate S1 (mean $\pm$ SD= $2.1\pm1.0$ cm posterior). 21 studies did not report using MEPs,  
336 but relied instead on visible twitches in the muscles of the hand (e.g., Amemiya et al.  
337 2017). These studies moved the coil a mean $\pm$ SD of  $1.6\pm1.2$ cm posterior to the M1  
338 hand area. In most studies, the researchers reported moving directly posterior

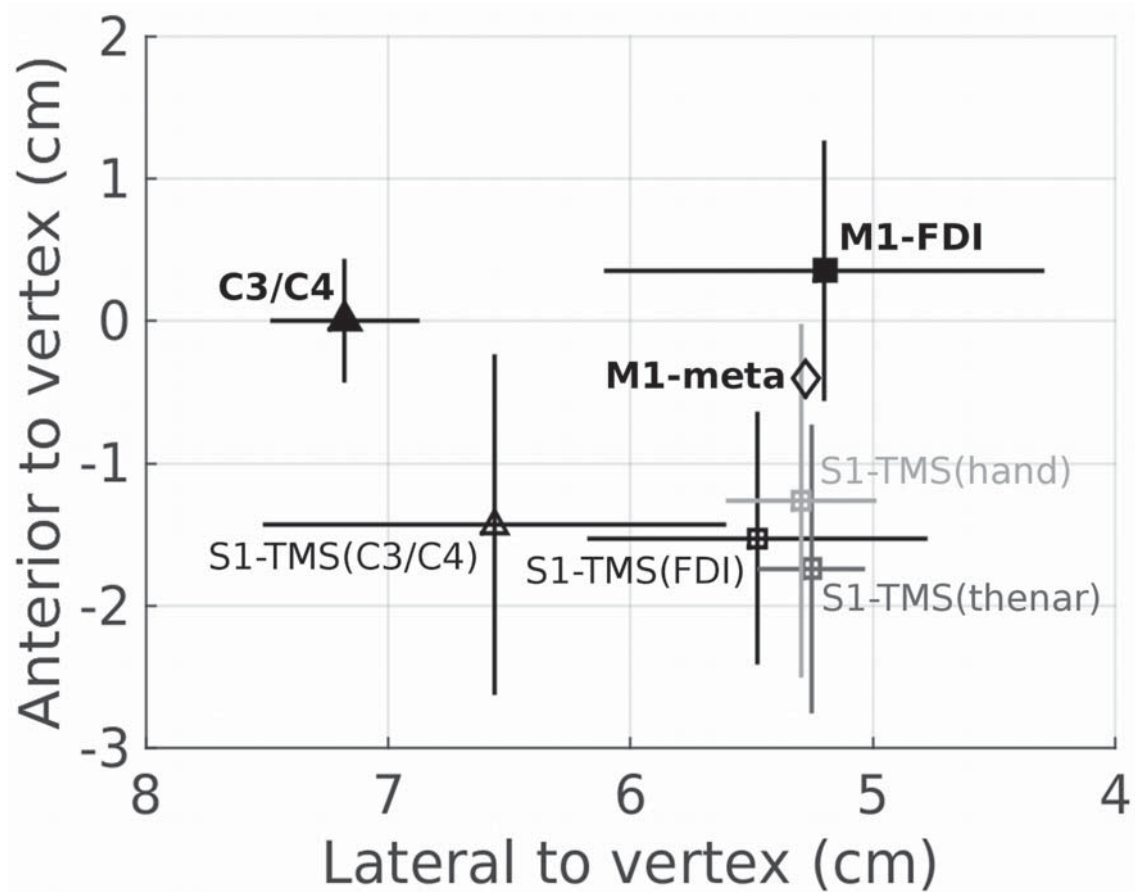
339 (parasagittally) to the motor location, while other researchers moved at an oblique  
340 angle away from the midline, reasoning that the central sulcus is oriented at  
341 approximately 45 degrees to the midline (e.g., Balslev et al. 2004). The estimated  
342 mean locations stimulated under these different strategies are depicted in Figure 1.  
343 These estimates used data about the likely scalp locations of M1-FDI and C3/C4  
344 obtained in our laboratory. These data are described below.

345

346

[FIGURE 1 ABOUT HERE]

347



348 *Figure 1. Systematic review of the locations stimulated in transcranial magnetic*  
349 *stimulation (TMS) studies of the hand area of primary somatosensory cortex (S1).*



350 *The grid shows locations lateral to the vertex, Cz(0,0) on the x-axis, and anterior to*  
351 *the vertex on the y-axis. The data points show mean±standard deviation (SD)*  
352 *locations measured or stimulated across the included studies (Table 1). Filled black*  
353 *square: Scalp location of primary motor cortex (M1) representation of the first dorsal*  
354 *interosseus (FDI) muscle of the hand, obtained from the HandLab database. Filled*  
355 *black triangle: Scalp location of the C3/C4 electroencephalographic electrode*  
356 *location obtained from the HandLab database. Black open triangle: Scalp location*  
357 *stimulated in TMS studies of S1 which use C3/C4 as a reference point (Table 2).*  
358 *Black open diamond: Scalp location of M1-FDI/thenar representation, obtained from*  
359 *non-systematic review (Table 3). Black open square: Scalp location stimulated in*  
360 *TMS studies of S1 which use the M1-FDI location as a reference point. Dark grey*  
361 *open square: Scalp location stimulated in TMS studies of S1 which use the M1-*  
362 *thenar location as a reference point. Light grey open square: Scalp location*  
363 *stimulated in TMS studies of S1 which use the M1 hand location (in general, usually*  
364 *without electromyography) as a reference point.*

365

366 A third approach to locate S1-hand has been to use MRI-guided neuronavigation.  
367 This was done in three main ways: Using a standard head and brain template and  
368 registering each participant's head to the template head (4 studies, e.g., Ruzzoli and  
369 Soto-Faraco, 2014), using individual structural MRI scans obtained from each  
370 participant (7 studies, e.g., Romaguère et al. 2005), using individual structural MRI  
371 scans with additional individual fMRI data (3 studies, e.g., Valchev et al. 2015).  
372 Seven additional studies reported using neuronavigation, but it was either not clear  
373 which of these three categories they used, or multiple approaches were used across

374 different sub-groups of participants. Only one study that used neuronavigation also  
375 reported coordinates of S1 relative to M1 (Tamè and Holmes, 2016).

376

377 ***Review of studies relating scalp and cortical anatomy***

378 In an appendix to a report on clinical EEG methods, Jasper (1958) reviewed four  
379 existing systems of EEG electrode positioning, and consolidated them into the 'Ten  
380 twenty' system of the International Federation. Cadavers and X-ray were used to  
381 register the EEG locations to the underlying brain anatomy. Positions C3/C4 are  
382 shown lying over the Rolandic fissure (see figure 6 in Jasper, 1958). Using MRI in 4  
383 participants, Towle and colleagues (1993) found C3/4 to be anterior to the central  
384 sulcus in five hemispheres, and posterior in three. They reported that the location  
385 C3'/C4' (also called CP3/CP4), which is several centimeters posterior to C3, was  
386 posterior to the central sulcus in all participants. Three later studies (Lagerlund et al.  
387 1993; Vitali et al. 2002; Okamoto et al. 2004) used MRI in 10 or more participants. All  
388 found that the brain underneath the C3/C4 location corresponded to the range of  
389 coordinates MNI( $\pm 51:57, -13:-23, 54:58$ ), with a left hemisphere weighted mean of  
390 MNI(-53,-18,57). The grey matter closest to this coordinate (e.g., MNI(-53,-17,55))  
391 corresponds in the Harvard-Oxford and Juelich (e.g., Eickhoff et al. 2005)  
392 probabilistic atlases to postcentral gyrus (62%), BA1 (88%), BA2 (4%), BA3b (2%),  
393 BA4p (1%), and BA4a (1%). Finally, Xiao et al. (2018) published the most detailed  
394 and systematic mapping study to date, involving 114 Chinese and 24 Caucasian  
395 participants. C3/C4 is positioned just posterior to the central sulcus, over the  
396 postcentral gyrus. These studies are summarised in Table 2.

397

398 Seven studies were found that mapped the locations of M1-FDI or M1-APB to the  
399 scalp and/or cortical surface. Excluding a single case study which produced a very  
400 different localization, the M1-FDI/ABP location was found to be at Cz(-5.9:-4.8,-  
401 0.8:0.5), approximately 5cm lateral to the vertex (Figure 1). Three studies registered  
402 the optimal location for M1-FDI/APB to the cortical surface, finding the cortical  
403 projection point at MNI(-40:-31,-22:-14,52:59), with a weighted left hemisphere mean  
404 of MNI(-38,-15,58). This coordinate corresponds in the Harvard-Oxford and Juelich  
405 probabilistic atlases to precentral gyrus (38%), postcentral gyrus (2%) BA6 (50%),  
406 BA4a (38%), BA3b (19%), BA1 (9%), and BA4p (4%). These studies are summarised  
407 in Table 3.

408

#### 409 ***Systematic review of FMRI of S1-hand***

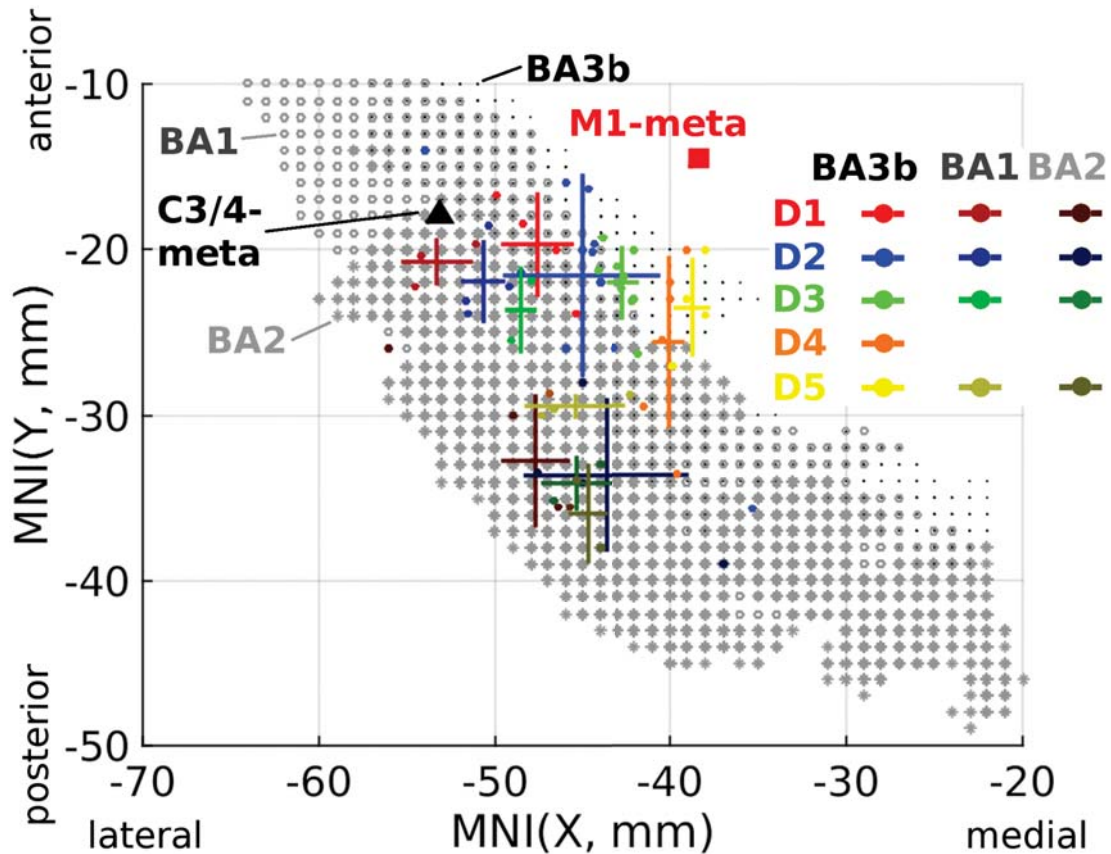
410 Of ninety-five studies reviewed, there were 216 reported coordinates relating to  
411 passive stimulation of the fingers, hand, and median nerve at the wrist. Some studies  
412 labeled the coordinates according to the likely Brodmann's areas (BA3b, BA1, BA2),  
413 but the majority used labels S1, SI, or postcentral gyrus. Juelich probabilistic atlases  
414 for BA3b, BA1, and BA2, in 1mm isotropic resolution in MNI152 space, were  
415 imported into Matlab. These maps had been thresholded at 50% likelihood for each  
416 brain area. The coordinates of the included studies were plot in 3D to check the  
417 distribution of data. Datapoints that were more than 2mm outside the 50% probability  
418 volumes were excluded. All remaining data were included. Averages for different  
419 hemispheres and reported Brodmann's areas are provided in Table 4, and a visual  
420 representation of the data is given in Figure 2. A full list of included studies, 3D  
421 figures, and all analysis data and scripts is available at <https://osf.io/c8nhj/>.

422

423

424

[FIGURE 2 ABOUT HERE]



425 Figure 2. Systematic review of the locations activated in functional magnetic  
426 resonance imaging (fMRI) studies of the hand area of primary somatosensory cortex  
427 (S1-hand). The data show locations in the standard Montreal Neurological Institute  
428 (MNI) coordinates, with mm right of the origin shown on the x-axis, and mm anterior  
429 to the origin on the y-axis. The small background symbols show the 50% probability  
430 volumes of the Juelich cytoarchitectural maps for S1: Black dots: Brodmann's area  
431 (BA) 3b, open dark grey circles: BA1, light grey asterisks: BA2. Large filled symbols  
432 show the locations of C3/C4 (filled black triangle) and primary motor cortex (M1)  
433 representation of the first dorsal interosseus (FDI) or thenar muscle (filled red

434 square), obtained from the systematic reviews. Filled colored circles show the  
435 reported MNI coordinates of individual studies included in the review, separated by  
436 cytoarchitectural area. Different colors show different digits (D1: red, D2: blue, D3:  
437 green, D4: orange, D5: yellow). The lightest tones are for BA3b data, mid-tones for  
438 BA1, and darkest tones for BA2. Horizontal and vertical colored lines show the  
439 means±standard deviations (SD) of the data, by digit and cytoarchitectural area.  
440 Data for the ring finger (D4) were reported only for BA3b. The key result is that the  
441 blue crosses are lateral to the red square – that S1-index is lateral, not directly  
442 posterior, to M1-FDI.

443

#### 444 **Relationship between TMS locations and FMRI locations of S1-hand**

445 Review of previous attempts to relate scalp and cortical anatomy revealed that the  
446 C3/C4 electrode location overlies the central sulcus, precentral gyrus, or postcentral  
447 gyrus, with a weighted mean coordinate for the cortical projection site of MNI(-53,-  
448 18,57). This site is 8mm lateral, 4mm anterior, and 7mm superior to the BA3b  
449 representation of S1-index, as determined by the systematic review. The scalp  
450 location of M1-FDI/APB across four studies was Cz(-5.3,0.0), and the likely cortical  
451 projection site was MNI(-38,-15,58). This is 7mm medial, 7mm anterior, and 8mm  
452 superior to the BA3b representation of S1-index.

453

454 The systematic reviews revealed very consistent strategies used to locate S1-index  
455 in TMS studies, namely moving an average of approximately 2cm posterior from M1-  
456 FDI. The systematic reviews also revealed that the cortical location of the index finger  
457 in FMRI studies of BA3b is likely 7mm lateral, 7mm posterior, and 8mm inferior to the

458 cortical location of M1-FDI. The representation of the index finger in BA1 is likely  
459 13mm lateral, 6mm posterior, and 8mm inferior to M1-FDI; and the index finger in  
460 BA2 is likely 5mm lateral, 18mm posterior, and 4mm inferior to M1-FDI. These  
461 distances are all measured within the brain. It is not yet known how these distances  
462 will convert to measurements taken from the scalp, nor how they relate to the optimal  
463 TMS coil position required to target S1-hand. These questions will be answered in a  
464 separate report.

465

## 466 **Discussion**

467 We systematically reviewed studies using transcranial magnetic stimulation and  
468 functional magnetic resonance imaging that targeted the hand area of the primary  
469 somatosensory cortex (S1-hand). Of 124 published TMS studies, the majority have  
470 used a heuristic to find S1-hand that involved finding the optimal location for  
471 stimulating the hand muscles (M1-hand), then moving the coil posteriorly, by a mean  
472 of approximately 2cm. Our own data, along with a review of similar studies (e.g.  
473 Sparing et al. 2008), shows that the optimal location for stimulating the M1  
474 representation of intrinsic hand muscles is approximately 4-6cm lateral and 0-1cm  
475 anterior or posterior to the vertex. For primary somatosensory cortex, on average,  
476 TMS studies targeting the hand area of S1 have therefore stimulated a location ~6cm  
477 lateral, and ~1.5cm posterior to the vertex (Figure 1).

478

479 FMRI studies have localised the index finger representation of Brodmann's BA3b in  
480 the left hemisphere at MNI(-45,-22,50), and of BA1 approximately 6mm lateral to  
481 that, at MNI(-51,-21,51). By co-registering data on the scalp position of M1-hand (M1-

482 meta in Figure 2) and C3/C4 into the same coordinate frame (i.e., the MNI template),  
483 the estimated locations of M1-hand and S1-hand can be compared. There is an  
484 orderly progression of the mean representation of the digits, with the little (D5) and  
485 ring finger (D4) representations in BA3b approximately 15mm posterior to M1-hand,  
486 and the thumb representation (D1) approximately 9mm lateral and 5mm posterior to  
487 M1-hand. These meta-analytic locations correspond well with the orderly  
488 topographies found within individual participants (e.g., Nelson & Chen 2008).

489

490 The heuristic of moving the TMS coil directly posterior to the M1 representation of the  
491 intrinsic hand muscles to locate the S1-hand representation therefore seems to be  
492 sub-optimal. This strategy is likely to be approximately correct if the TMS target is the  
493 BA3b representation of the little and ring fingers, but these digits are rarely targeted  
494 (only two out of the 87 reviewed studies that presented tactile stimuli to the fingers  
495 targeted these digits – Amassian et al. 1991; Knecht et al. 2003). By contrast, the  
496 largest number of studies used the M1 representation of intrinsic hand muscles to  
497 target the S1 representation of the index finger (36 of the 87 studies presented tactile  
498 stimuli on the index finger). Despite the predominance of this strategy, the systematic  
499 review data suggest that S1-index is lateral and slightly posterior to M1-hand.

500

501 The conclusion that S1-hand is lateral to M1-hand is supported by studies in which  
502 both M1 and S1 representations are measured together. Blatow and colleagues  
503 (2011) applied passive pneumatic stimulation to the index finger and thumb of 16  
504 participants, as well as asking them to make finger-thumb opposition movements for  
505 digits 1-5. The peak BOLD response in their active movement task (after converting

506 their coordinates to MNI space) puts M1-hand at MNI(-39,-29,58), and S1-hand in the  
507 sensory task 11mm laterally, 2mm anteriorly, and 6mm inferiorly, at MNI(-50,-27,52).  
508 Their figure 2b clearly shows S1-hand lateral to M1-hand. Similar conclusions were  
509 reached by Schellekens et al. (2018) using population receptive field methods, and  
510 by Tamè & Holmes (2016), who reported that the S1-index representation was 11mm  
511 lateral, 7mm posterior, and 11mm inferior to the M1 representation of FDI, as  
512 measured using TMS-evoked MEPs in that muscle.

513

514 Given that moving the TMS coil posterior to the M1-hand representation does not  
515 seem optimal to target S1-hand, the question arises as to why this method seems to  
516 have become the default. Indeed, this method is still commonly relied upon, with one  
517 recent paper stating: “*A large body of evidence shows that the hand area in the*  
518 *somatosensory cortex can be successfully targeted by positioning the coil 1–4 cm*  
519 *posterior to the motor hotspot*” (Gallo et al. 2018, p19). The earliest TMS studies of  
520 S1 (e.g., Cohen et al. 1991; Seyal et al. 1992, 1993) positioned the TMS coil over the  
521 C3/C4 electrode position. These studies presumably relied on evidence showing that  
522 the C3/C4 location lay approximately over the central sulcus (Jasper, 1958; Towle et  
523 al. 1993; Table 2). Indeed, studies relating the C3/C4 position to the underlying brain  
524 surface gave an estimated location of the C3/C4 projection point of MNI(-53,-18,57)  
525 (Figure 2). This cortical projection point of C3/C4 is just 6.6mm from the BA1  
526 representation of the thumb.

527

528 Since the C3/C4 projection point is so close to the likely representation of thumb and  
529 index fingers in BA1 and BA3b, and the available evidence suggests that finger



530 representations in S1 are lateral to those in M1, why is *2cm posterior to the M1-hand*  
531 *location* the dominant reference point for TMS studies of S1-hand? While the  
532 literature is not clear on this point, one possibility is that, following Towle et al. (1993),  
533 who reported that the C3'/C4' electrode location was posterior to the central sulcus in  
534 all four of their participants, subsequent researchers have used C3'/C4' to ensure that  
535 they were on the posterior side of the central sulcus. C3'/C4' (also labeled CP3/CP4)  
536 is halfway between C3 and P3, which, from our scalp measurements is about 3.6cm  
537 posterior to C3/C4. Relatively few studies have used a site as posterior as this to  
538 target S1 (e.g., McKay et al. 2003; Restuccia et al. 2007). Other researchers have  
539 located C3'/C4' only about 1.5cm posterior to C3/C4 (Pascual-Leone & Torres, 1993).  
540 Some researchers state that the C3/C4 location is several centimeters posterior to  
541 the optimal location to stimulate M1 (Feurra et al. 2011; Koch et al. 2006; McKay et  
542 al. 2003; Nardone et al. 2015, 2016), which from our scalp measurements does not  
543 seem correct. Other researchers state that C3/C4 is the approximate scalp location of  
544 the M1-hand representation (e.g., Fiorio & Haggard 2005; McKay et al. 2003). It  
545 seems that, at some point, the original heuristic of 'posterior to C3/C4' has changed  
546 into the heuristic 'posterior to M1-hand'. We did not find an empirical justification for  
547 this change. At present, then, selective citation of the literature can be used to justify  
548 a number of different strategies. In systematically reviewing this literature, it is clear  
549 that there is very little agreement among researchers about the relative scalp  
550 locations of C3/C4, C3'/C4', and their relationship to the underlying representations of  
551 M1-hand, and S1-hand. The data reviewed here show that these areas are all  
552 several centimeters apart. In the following, we consider two additional reasons why  
553 researchers might have chosen to move the TMS coil posteriorly from M1-hand to

554 target S1-hand.

555

556 Using TMS to evoke MEPs in hand muscles provides a potentially very reliable  
557 functional localiser for M1-hand. Localising M1-hand functionally is likely better than  
558 relying on scalp measurements alone. Once M1-hand has been localised,  
559 researchers have often justified moving the coil posteriorly to M1-hand in order to  
560 ensure that muscle twitches evoked by stimulating over M1 would not interfere with  
561 the intended effects of TMS over S1 (e.g., Convento et al. 2018; see also Holmes &  
562 Tamè, 2018). This strategy can be criticized on two grounds.

563

564 First, M1 and S1 are adjacent and anatomically contiguous in the brain. For the  
565 purposes of TMS, stimulation of the posterior bank of the precentral sulcus (e.g.,  
566 BA4p, primary motor cortex) and the anterior bank of the postcentral sulcus (e.g.,  
567 BA3b, primary somatosensory cortex) is very likely to occur simultaneously. Selective  
568 stimulation of particular sub-areas of primary sensory (e.g., BA3a vs. BA3b) or motor  
569 cortex (BA4a vs. BA4p) is likely to require detailed and careful work to optimise  
570 precisely the necessary location, orientation, intensity, and TMS pulse pattern (e.g.,  
571 Hamada et al., 2012). By comparison to the strategy for selectively stimulating S1 but  
572 not M1, TMS studies focusing on M1 (or other brain areas) have not argued for  
573 moving the coil anteriorly in order to prevent simultaneous stimulation of S1, even  
574 though it is likely that S1 stimulation directly affects M1 activity, for example, as  
575 shown by the short-afferent-inhibition paradigm (Tamè et al. 2015; Turco et al. 2018).  
576 Rather, specific stimulation of M1 must be deduced from the effects of TMS, and  
577 these may depend on the timing, intensity, orientation, or pattern of TMS impulses,

578 on connectivity with other areas, or on other factors that allow M1 involvement to be  
579 determined.

580

581 Second, in our previous experiments using fMRI-guided neuronavigated TMS over  
582 S1, while TMS has indeed evoked muscle twitches in many participants, the  
583 amplitude of these twitches did not correlate with the effects of TMS on tactile  
584 perception (Tamè and Holmes, 2016). We suggest that there is no necessary reason  
585 to attempt to avoid the side-effects of M1 stimulation when targeting S1. Rather,  
586 researchers should stimulate S1 as directly as possible, measure any muscle  
587 contractions that result, and test whether these contractions interfere or correlate with  
588 somatosensory perception or other measures. To this end, it may be that different coil  
589 orientations should be used to stimulate S1-hand as compared to M1-hand (e.g.,  
590 Pascual-Leone et al. 1994; Raffin et al. 2015). Future studies will need to follow-up  
591 on these reports of the optimal coil orientation for interfering with somatosensory  
592 perception. Once we are more certain about the location of S1-hand, we can then  
593 begin to study how S1-hand and somatosensory perception respond in detail to  
594 systematic changes in TMS coil position and orientation, and TMS pulse intensity,  
595 frequency, and pattern.

596

597 It may also be argued that, by moving the TMS coil 2cm posterior to M1-hand,  
598 researchers were specifically targeting the little or ring finger representations in BA3b  
599 or BA1, or the largely-overlapping finger representations in BA2 (Figure 2). 2cm  
600 directly posterior to M1-hand (i.e., MNI(-38,-35,58) – compare the location stimulated  
601 by Ku et al. 2015: MNI(-34,-36,51)) is likely on the posterior bank of the postcentral

602 gyrus (cytoarchitectural probability: 39%) or superior parietal lobule (17%), and may  
603 include parts of BA3b (52%), BA2 (46%), BA1 (21%), BA7 (20%), BA4p (12%) BA5  
604 (5%) or BA4a (4%). BA1 and BA2 are less clearly somatotopically organized than  
605 BA3b (Martuzzi et al. 2014; see Figure 2). It is therefore possible that TMS over a  
606 region approximately 2cm behind M1-hand may be sufficient for targeting higher-  
607 order and less topographic representations of the hand in S1. Although we have not  
608 done the necessary systematic review or experiments to determine which part of S1  
609 is 2cm posterior to the M1-hand location, it is most likely to be a part of S1 that  
610 represents the forearm, upper arm, and/or shoulder (e.g., Blankenburg et al., 2006;  
611 Figure 2).

612

### 613 *Scope and recommendations*

614 This review was limited to assessing the scalp locations that previous TMS studies  
615 have assumed to correspond to S1-hand, as well as the brain locations activated  
616 during passive somatosensory stimulation of the hand. Explicitly relating the TMS  
617 scalp measurements and the fMRI brain measurements is beyond the scope of this  
618 review. In an accompanying experimental paper (Holmes et al., under review), we  
619 systematically map the effect of TMS on tactile perception, provide a probabilistic  
620 atlas of the central sulcus, and systematically measure the location of S1-hand using  
621 individual fMRI-guided neuronavigation. From the systematic reviews reported here,  
622 we can make three general recommendations.

623

624 First, we recommend that all TMS studies should use as much of the available  
625 evidence as possible to guide and justify their choice of target scalp locations,

626 including systematic review, meta-analysis, FMRI, M/EEG, scalp measurements, and  
627 behavioral data. By selectively citing the literature, quite a wide range of strategies  
628 for localising a TMS target can appear evidence-based. In the reviewed literature, we  
629 were unable to find any empirical evidence to support the most commonly-reported  
630 strategy for localising S1-hand in TMS studies, that is, moving 2cm posterior from the  
631 M1-hand representation. While the distances involved are relatively small (i.e., 2cm,  
632 relative to a typical TMS coil diameter of 7cm), researchers studying MEPs elicited by  
633 TMS over M1 know just how sensitive the measurements can be to relatively small  
634 changes in TMS coil position and orientation. More accurate positioning of the TMS  
635 coil should increase the effect sizes of the phenomena we set out to measure.

636

637 Second, we recommend that all TMS studies systematically measure and report their  
638 participants' head measurements and the scalp locations stimulated, using a  
639 common reference frame. Very few studies reported scalp measurements. For sites  
640 close to the vertex, measurements lateral and anterior in a Cartesian system relative  
641 to the vertex may be sufficient, although a polar system may be superior. For sites  
642 further from the vertex, the reference point could be relative to another 10:20  
643 electrode location (e.g., C3/C4; Pz). If a functional localiser is available, such as  
644 MEPs elicited from M1-FDI, then careful mapping of that functional location is  
645 required prior to reporting the target location relative to that reference.

646

647 Finally, from the evidence presented here, we suggest that the representation of the  
648 index finger in BA3b and BA1 is likely to be around 1cm lateral, and 0.5cm posterior  
649 to M1-FDI, as measured in the brain. These distances, particularly the lateral

650 distance, are likely to be underestimates relative to the equivalent distances  
651 measured along the scalp, due to the distance between the scalp and the brain, and  
652 the curvature of the scalp. The scalp localisation of S1-index is addressed by Holmes  
653 et al. (under review).

654 **Online data**

655 Raw data, supplementary results, data sheet, (<https://osf.io/c8nhj/>).

656

657 **References**

- 658 Amassian VE, Somasundaram M, Rothwell JC, Britton TC, Cracco JB, Cracco RQ,  
659 Maccabee PJ, Day B L. Paraesthesias are elicited by single pulse, magnetic coil  
660 stimulation of motor cortex in susceptible humans. *Brain* 114, 2505—2520,  
661 1991.
- 662 Amemiya T, Beck B, Walsh VZ, Gomi HR, Haggard P. Visual area V5/hMT+  
663 contributes to perception of tactile motion direction: a TMS study. *Sci. Rep.* 7,  
664 40937, 2017.
- 665 Balslev D, Christensen LO, Lee J, Law I, Paulson OB, Miall RC. Enhanced  
666 accuracy in novel mirror drawing after repetitive transcranial magnetic  
667 stimulation-induced proprioceptive deafferentation. *J. Neurosci.* 24, 9698—  
668 9702, 2004.
- 669 Barker AT, Jalilnous R, Freeston IL. Noninvasive magnetic stimulation of human  
670 motor cortex. *Lancet* 1, 1106—1107, 1985.
- 671 Blatow M, Reinhardt J, Riffel K, Nennig E, Wengenroth M, Stippich C (2011) Clinical  
672 functional mri of sensorimotor cortex using passive motor and sensory  
673 stimulation at 3 tesla. *J. Magn. Reson. Imag.* 34(2), 429—437
- 674 Borghetti D, Sartucci F, Petacchi E, Guzzetta A, Piras MF, Murri L, Cioni G.  
675 Transcranial magnetic stimulation mapping: A model based on spline  
676 interpolation. *Brain Res. Bull.* 77, 143—148, 2008.
- 677 Boroojerdi B, Foltys H, Krings T, Spetzger U, Thron A, Töpper R. Localization of the

678 motor hand area using transcranial magnetic stimulation and functional  
679 magnetic resonance imaging. *Clin. Neurophysiol.* 110, 699—704, 1999.

680 Cohen LG, Bandinelli S, Sato S, Kufta C, Hallett M. Attenuation in detection of  
681 somatosensory stimuli by transcranial magnetic stimulation.  
682 Electroencephalography *Clin. Neurophysiol.* 81, 366—376, 1991.

683 Convento S, Rahman S, Yau JM. Selective attention gates the interactive crossmodal  
684 coupling between perceptual systems. *Curr. Biol.* 28, 746—752, 2018.

685 Cushing H. A note upon the faradic stimulation of the postcentral gyrus in conscious  
686 patients. *Brain* 32, 44—54, 1909.

687 Cutini S, Scatturin P, Zorzi M. A new method based on ICBM152 head surface for  
688 probe placement in multichannel FNIRS. *NeuroImage* 54, 919—927, 2011.

689 Eickhoff SB, Stephan KE, Mohlberg H, Grefkes CB, Fink GR, Amunts K, Zilles K. A  
690 new SPM toolbox for combining probabilistic cytoarchitectonic maps and  
691 functional imaging data. *NeuroImage* 25(4): 1325–1335, 2005.

692 Enomoto H, Hanajima R, Yuasa K, Mochizuki H, Terao Y. Decreased sensory cortical  
693 excitability after 1 Hz rTMS over the ipsilateral primary motor cortex. *Clin.*  
694 *Neurophysiol.* 112, 2154—2158, 2001.

695 Feurra M, Paulus WE, Walsh VZ, Kanai R. Frequency specific modulation of human  
696 somatosensory cortex. *Front. Psychol.* 2: 13, 2011.

697 Gallo S, Paracampo R, Müller-Pinzler L, Severo MC, Blömer L, Fernandes-Henriques  
698 C, Henschel A, Lammes B, Maskaljunas T, Suttrup J, Avenanti A, Keysers C,  
699 Gazzola V. The causal role of the somatosensory cortex in prosocial behaviour.  
700 *e-Life*, 7: e32740, 2018.

701 Geyer S, Schleicher A, Zilles K. Areas 3a, 3b, and 1 of human primary



702 somatosensory cortex: Part 1. Micro structural organization and interindividual  
703 variabilities. *NeuroImage* 10, 63—83, 1999.

704 Hamada M, Murase N, Hasan A, Balaratnam M, Rothwell JC. The role of interneuron  
705 networks in driving human motor cortical plasticity. *Cereb. Cortex*, 23: 1593–  
706 1605, 2013.

707 Harris JA, Miniussi C, Harris IM, Diamond ME. Transient storage of a tactile memory  
708 trace in primary somatosensory cortex. *J. Neurosci.* 22, 8720—8725, 2002.

709 Hayward KS, Schmidt J, Lohse KR, Peters S, Bernhardt J, Lannin NA, Boyd LA. Are  
710 we armed with the right data? Pooled individual data review of biomarkers in  
711 people with severe upper limb impairment after stroke. *NeuroImage Clin.* 15: 53  
712 – 55, 2016

713 Hiremath SV, Tyler-Kabara EC, Wheeler JJ, Moran DW, Gaunt RA, Collinger JL,  
714 Foldes ST, Weber DJ, Chen W, Boninger ML, Wang W. Human perception of  
715 electrical stimulation on the surface of somatosensory cortex. *PLoS ONE* 12,  
716 e176020, 2017.

717 Hlustík P, Solodkin A, Gullapalli RP, Noll DC, Small SL. Somatotopy in human  
718 primary motor and somatosensory hand representations revisited. *Cereb.*  
719 *Cortex*, 11: 312–321, 2001.

720 Holmes NP, Meteyard L. Subjective annoyance of TMS predicts reaction times  
721 differences in published studies. *Front. Psychol.* 9, 1989, 2018

722 Holmes NP, Tamè L, Beeching P, Medford M, Rakova M, Stuart A, Zeni S. Locating  
723 primary somatosensory cortex in human brain stimulation studies: Experimental  
724 evidence. *J. Neurophysiol.* Under review.

725 Holmes NP, Tamè L. Multisensory perception: magnetic disruption of attention in

726 human parietal lobe. *Curr. Biol.* 28, R259—261, 2018.

727 Jasper H. Report of the committee on methods of clinical examination in  
728 electroencephalography: 1957. *Electroencephalography Clin. Neurophysiol.* 10,  
729 370—375, 1958.

730 Knecht S, Ellger T, Breitenstein C, Bernd Ringelstein E, Henningsen H. Changing  
731 cortical excitability with low-frequency transcranial magnetic stimulation can  
732 induce sustained disruption of tactile perception. *Biol. Psychiat.* 53(2-3): 175–  
733 179, 2003.

734 Koch G, Franca M, Albrecht U, Caltagirone C, Rothwell JC. Effects of paired pulse  
735 TMS of primary somatosensory cortex on perception of a peripheral electrical  
736 stimulus. *Exp. Brain Res.* 172(3): 416–424, 2006

737 Koessler L, Maillard L, Benhadid A, Vignal JP, Felblinger J, Vespignani H, Braun M.  
738 Automated cortical projection of EEG sensors: anatomical correlation via the  
739 international 10–10 system. *NeuroImage* 46, 64—72, 2009.

740 Ku Y, Zhao D, Hao N, Hu Y, Bodner M, Zhou Y. Sequential roles of primary  
741 somatosensory cortex and posterior parietal cortex in tactile-visual cross-modal  
742 working memory: a single-pulse transcranial magnetic stimulation (spTMS)  
743 study. *Brain Stim.* 8(1): 88–91, 2015.

744 Lagerlund TD, Sharbrough FW, Jack CR, Erickson BJ, Strelow DC, Cicora KM,  
745 Busacker NE. Determination of 10 – 20 system electrode locations using  
746 magnetic resonance image scanning with markers. *Electroencephalography*  
747 *Clin. Neurophysiol.* 86, 7—14, 1993.

748 Martuzzi R, van der Zwaag W, Farthouat J, Gruetter R, Blanke O. Human finger  
749 somatotopy in areas 3b, 1, and 2: a 7T fMRI study using a natural stimulus.

750 *Hum. Brain Mapp.* 35(1): 213–226, 2014.

751 McKay DR, Ridding MC, Miles TS. Magnetic stimulation of motor and somatosensory  
752 cortices suppresses perception of ulnar nerve stimuli. *Int. J. Psychophysiol.*  
753 48(1): 25–33, 2003.

754 Meteyard L, Holmes NP. TMS SMART – scalp mapping of annoyance ratings and  
755 twitches caused by transcranial magnetic stimulation. *J. Neurosci. Meth.* 299:  
756 34–44, 2018.

757 Nardone R, De Blasi P, Höller Y, Taylor AC, Brigo F, Trinka E. Effects of theta burst  
758 stimulation on referred phantom sensations in patients with spinal cord injury.  
759 *NeuroReport*, 27(4): 209–212, 2016

760 Nardone R, Langthaler PB, Höller Y, Bathke A, Frey VN, Brigo F, Trinka E.  
761 Modulation of non-painful phantom sensation in subjects with spinal cord injury  
762 by means of rtms. *Brain Res. Bull.*, 118: 82–86, 2015.

763 Nelson AJ, Chen R. Digit somatotopy within cortical areas of the postcentral gyrus in  
764 humans. *Cereb. Cortex* 18(10): 2341–2351, 2008.

765 Niskanen E, Julkunen P, Säisänen L, Vanninen R, Karjalainen P, Könönen M. Group-  
766 level variations in motor representation areas of thenar and anterior tibial  
767 muscles: navigated transcranial magnetic stimulation study. *Hum. Brain Mapp.*  
768 31(8): 1272–1280, 2010.

769 Okamoto M, Dan H, Sakamoto K, Takeo K, Shimizu K, Kohno S, Oda I, Isobe S,  
770 Suzuki T, Kohyama K, Dan I. Three-dimensional probabilistic anatomical cranio-  
771 cerebral correlation via the international 10–20 system oriented for transcranial  
772 functional brain mapping. *NeuroImage* 21(1): 99–111, 2004.

773 Pascual-Leone A, Cohen A, Brasil-Neto JP, Valls-Solé J, Hallett M. Differentiation of

774 sensorimotor neuronal structures responsible for induction of motor evoked  
775 potentials, attenuation in detection of somatosensory stimuli, and induction of  
776 sensation of movement by mapping of optimal current directions.  
777 *Electroencephalography Clin. Neurophysiol.* 93(3): 230–236, 1994.

778 Pascual-Leone A, Torres F. Plasticity of the sensorimotor cortex representation of the  
779 reading finger in Braille readers. *Brain* 116(1): 39–52, 1993.

780 Penfield WG, Boldrey E. Somatic motor and sensory representation in the cerebral  
781 cortex of man as studied by electrical stimulation. *Brain* 60(4): 389–443, 1937.

782 Raffin E, Pellegrino G, di Lazzaro V, Thielscher A, Siebner HR. Bringing transcranial  
783 mapping into shape: sulcus-aligned mapping captures motor somatotopy in  
784 human primary motor hand area. *NeuroImage* 120: 164–175, 2015.

785 Ragert P, Dinse HR, Pleger B, Wilimzig C, Frombach E, Schwenkreis P. Combination  
786 of 5 Hz repetitive transcranial magnetic stimulation (rTMS) and tactile  
787 coactivation boosts tactile discrimination in humans. *Neurosci. Lett.* 348(2):  
788 105–108, 2003.

789 Restuccia DW, Ulivelli M, De Capua A, Bartalini S, Rossi S. Modulation of high-  
790 frequency (600 Hz) somatosensory-evoked potentials after rTMS of the primary  
791 sensory cortex. *Eur. J. Neurosci.* 26(8): 2349–2358, 2007.

792 Romaiguère P, Calvin S, Roll J. Transcranial magnetic stimulation of the  
793 sensorimotor cortex alters kinaesthesia. *NeuroReport* 16(7): 693–697, 2005.

794 Rossi S, Hallett M, Rossini PM, Pascual-Leone A, The Safety of TMS Consensus  
795 Group. Safety, ethical considerations, and application guidelines for the use of  
796 transcranial magnetic stimulation in clinical practice and research. *Clin.*  
797 *Neurophysiol.* 120(12): 2008–2039, 2009.

798 Ruohonen JO, Ravazzani P, Ilmoniemi RJ, Galardi G, Nilsson J, Panizza M, Amadio  
799 S, Grandori F, Comi G. Motor cortex mapping with combined MEG and  
800 magnetic stimulation. *Electroencephalography Clin. Neurophysiol.* 46: 317–322,  
801 1996.

802 Ruzzoli M, Soto-Faraco S. Alpha stimulation of the human parietal cortex attunes  
803 tactile perception to external space. *Curr. Biol.* 24(3): 329–332, 2014.

804 Schellekens W, Petridou N, Ramsey NF. Detailed somatotopy in primary motor and  
805 somatosensory cortex revealed by Gaussian population receptive fields.  
806 *NeuroImage*, 179: 337–347, 2018.

807 Seyal M, Browne JK, Masuoka LK, Gabor AJ. Enhancement of the amplitude of  
808 somatosensory evoked potentials following magnetic pulse stimulation of the  
809 human brain. *Electroencephalography Clin Neurophysiol* 88(1): 20–27, 1993.

810 Seyal M, Masuoka LK, Browne JK. Suppression of cutaneous perception by  
811 magnetic pulse stimulation of the human brain. *Electroencephalography Clin.*  
812 *Neurophysiol.* 85(6): 397–401, 1992.

813 Siebner HR, Willloch F, Peller M, Auer C, Boecker H, Conrad B, Bartenstein P.  
814 Imaging brain activation induced by long trains of repetitive transcranial  
815 magnetic stimulation. *NeuroReport* 9(5): 943–948, 1998.

816 Sparing R, Buelte D, Meister IG, Paus T, Fink GR. Transcranial magnetic stimulation  
817 and the challenge of coil placement: a comparison of conventional and  
818 stereotaxic neuronavigational strategies. *Hum. Brain Mapp.* 29(1): 82–96, 2008.

819 Sugishita M, Takayama Y. Paraesthesia elicited by repetitive transcranial magnetic  
820 stimulation of the postcentral gyrus. *NeuroReport* 4(5): 569–570, 1993.

821 Talairach J, Tournoux P. *Co-planar Stereotaxic Atlas of the Human Brain: 3-*

822        *Dimensional Proportional System: An Approach to Cerebral Imaging*. Thieme,  
823        Stuttgart

824 Tamè L, Braun C, Holmes NP, Farnè A, Pavani F. Bilateral representations of touch in  
825        the primary somatosensory cortex. *Cogn. Neuropsychol.* 33(1-2): 48–66, 2016.

826 Tamè L, Holmes NP. Involvement of human primary somatosensory cortex in  
827        vibrotactile detection depends on task demand. *NeuroImage* 138: 184–196,  
828        2016.

829 Tamè L, Pavani F, Braun C, Salemmè R, Farnè A, Reilly KT. Somatotopy and  
830        temporal dynamics of sensorimotor interactions: evidence from double afferent  
831        inhibition. *Eur. J. Neurosci.* 41(11): 1459–1465, 2015.

832 Tegenthoff M, Ragert P, Pleger B, Schwenkreis P, Förster A, Nicolas V, Dinse HR.  
833        Improvement of tactile discrimination performance and enlargement of cortical  
834        somatosensory maps after 5 Hz rTMS. *PLoS Biol.* 3(11): e362, 2005.

835 Towle VL, Bolaños J, Suarez D, Tan KK, Grzeszczuk R, Levin DN, Cakmur R, Frank  
836        SA, Spire JP. The spatial location of EEG electrodes: locating the best-fitting  
837        sphere relative to cortical anatomy. *Electroencephalography Clin. Neurophysiol.*  
838        86(1): 1–6, 1993.

839 Turco CV, El-Sayes J, Savoie MJ, Fassett HJ, Locke MB, Nelson AJ. Short- and long-  
840        latency afferent inhibition; uses, mechanisms and influencing factors. *Brain*  
841        *Stim.* 11(1): 59–74, 2018.

842 Valchev N, Ćurčić-Blake B, Renken RJ, Avenanti A, Keysers C, Gazzola V, Maurits  
843        NM. CTBS delivered to the left somatosensory cortex changes its functional  
844        connectivity during rest. *NeuroImage* 114: 386–397, 2015.

845 Vitali P, Avanzini G, Caposio L, Fallica E, Grigoletti L, Maccagnano E, Villani F.

846 Cortical location of 10–20 system electrodes on normalized cortical mri  
847 surfaces. *Int. J. Bioelectromagn.* 4(2): 147–148, 2002.

848 Weiss C, Nettekoven C, Rehme AK, Neuschmelting V, Eisenbeis A, Goldbrunner R,  
849 Grefkes CB. Mapping the hand, foot and face representations in the primary  
850 motor cortex — retest reliability of neuronavigated tms versus functional mri.  
851 *NeuroImage* 66: 531–542, 2013.

852 Wilson SA, Thickbroom GW, Mastaglia FL. Transcranial magnetic stimulation  
853 mapping of the motor cortex in normal subjects. The representation of two  
854 intrinsic hand muscles. *J. Neurol. Sci.* 118(2): 134–144, 1993.

855 Xiao X, Yu X, Zhang Z, Zhao Y, Jiang Y, Li Z, Yang Y, Zhu C. Transcranial brain atlas.  
856 *Sci. Adv.* 4(9): eaar6904, 2018

857 Yoursy TA, Schmid UD, Alkadhi H, Schmidt D, Peraud A, Buettner A, Winkler PA.  
858 Localization of the motor hand area to a knob on the precentral gyrus: A new  
859 landmark. *Brain* 120(1): 141–157, 1997.

860 Zilles K, Kawashima RE, Dabringhaus A, Fukuda H, Schormann T. Hemispheric  
861 shape of European and Japanese brains: 3-D MRI analysis of intersubject  
862 variability, ethnical, and gender differences. *NeuroImage* 13(2): 262–271, 2001.

**Table 1: Systematic review of approximate scalp locations stimulated in 117 TMS studies of S1-hand**

Reference	N*	Relative to Reference (cm)		Relative to Cz (cm)†	
		Lateral	Anterior	Lateral	Anterior
<b>C3/C4</b>	16	0.0±0.0 (0.0:0.0)	-1.5±1.2 (-3.6:0.0)	-6.6±0.9 (-7.2:-5.2)	-1.4±1.2 (-3.6:0.4)
<b>FDI</b>	43	-0.3±0.7 (-3.0:0.0)	-1.9±0.9 (-3.0:0.0)	-5.5±0.7 (-8.2:-5.2)	-1.5±0.9 (-2.7±0.4)
<b>Thenar</b>	16	-0.1±0.2 (-0.9:0.0)	-2.1±1.0 (-4.0:0.0)	-5.3±0.2 (-6.1:-5.2)	-1.7±1.0 (-3.7:0.4)
<b>Hand/other</b>	21	-0.1±0.3 (-1.0:0.0)	-1.6±1.2 (-4.0:0.0)	-5.3±0.3 (-6.2:-5.2)	-1.3±1.2 (-3.7:-0.4)
<b>Navigated‡</b>	21	-	-	-	-

Data are Means±SD (min:max). \* Number of studies. Location data are not weighted by study sample-size. † Approximate measures, based on estimated population means reported below; ‡ Most neuronavigated studies did not report any coordinates, so no summary data are available.



**Table 2: Nonsystematic review of C3/C4 location**

Study	Methods	N	C3/C4*
Jasper 1958	Cadavers, X-rays	?	Over CS
Towle et al. 1993	MRI-EEG	4	Anterior to CS (5 hemispheres) Posterior to CS (3 hemispheres)
Lagerlund et al. 1993	MRI-EEG	10	45.6° lateral from Cz
Vitali et al. 2002	MRI-EEG	10†	M=MNI(-57,-13,54) SD=MNI(5,13,6)
Okamoto et al. 2004	MRI-EEG	17	M=MNI(-53,-16,58) SD=8; over postcentral gyrus
Koessler et al. 2009	MRI-EEG	16	MNI(-51,-23,57)‡
Cutini et al. 2011	MRI-EEG	(model)	MNI(-53,-11,49)
Xiao et al. 2018	MRI-EEG	114+24	Postcentral gyrus

C3/C4: anatomical location(s) of this electrode position; CoG: center of gravity; CS: central sulcus; Cz: vertex; M: Mean; MNI: Montreal Neurological Institute 152 template brain; N: Number of participants or brains; SD: Standard Deviation. \* Right hemisphere X-coordinates, if given, were inverted and averaged with left hemisphere (left-right differences were minimal); † Patients with epilepsy. ‡ Converted from Talairach and Tournoux coordinates.

**Table 3. Non-systematic review of M1-Hand scalp and brain location**

Study	TMS Methods	N	M1*
Wilson et al 1993	M1-APB CoG M1-ADM CoG	10	Cz(-5.9,0.5) Cz(-5.4,0.4)
Ruohonen et al 1996	MRI-MEG-TMS M1-APB M1-ADM	1	Precentral gyrus Cz(-3.0,2.0)
Boroojerdi et al 1999	FMRI-TMS M1-APB/FDI	4	Cz(-5.5,0.25)
Borghetti et al 2008	M1-ADM Median M1-ADM CoG	10	Cz(-4.5,0.0) Cz(-4.9,-0.8)
Sparing et al 2008	(Meta-analysis) M1-FDI Max	10	MNI(-31,-22,52) Cz(-4.8,-0.8)
Niskanen et al 2010	M1-APB	59	MNI(-38,-14,58)
Raffin et al 2015	MRI, M1-FDI	13	M=MNI(-40,-17,59) SD=MNI(10,7,24)

Cz: vertex; M: Mean; MNI: Montreal Neurological Institute 152 template brain; N: Number of participants or brains; SD: Standard Deviation. \* Right hemisphere X- coordinates, if given, were inverted and averaged with left hemisphere (left-right differences were minimal); CoG: Centre of Gravity

**Table 4: Weighted mean±SD reported S1 MNI coordinates across the reviewed studies**

Body	BA	Hem	N datapoints				MNI Coordinate means and SDs								
			Studies		People		X			Y			Z		
			Ms	SDs	Ms	SDs	M	SD <sub>M</sub>	SD <sub>P</sub>	M	SD <sub>M</sub>	SD <sub>P</sub>	M	SD <sub>M</sub>	SD <sub>P</sub>
Thumb (D1)	3b	L	4	4	52	52	-48.0	1.96	7.00	-19.0	3.04	4.27	47.3	3.25	6.25
		R	4	4	58	58	47.4	1.70	3.84	-18.3	2.81	2.86	45.7	0.25	3.79
	1	L	3	3	37	37	-52.8	1.92	2.41	-20.5	1.33	4.17	50.9	2.66	3.57
		R	6	5	98	61	53.9	3.40	3.28	-19.4	3.66	3.76	50.4	3.86	3.58
	2	L	2	2	9	9	-47.2	1.84	27.9	-33.9	3.89	5.42	56.5	4.53	7.13
		R	2	2	15	15	54.7	0.25	5.97	-24.8	2.43	4.60	48.5	1.29	5.74
Index (D2)	3b	L	11	5	136	81	-45.2	4.39	4.47	-21.6	6.00	2.87	49.8	5.30	4.52
		R	5	4	71	58	44.5	0.63	3.36	-19.9	3.41	2.98	50.0	1.00	2.93
	1	L	4	3	46	34	-50.8	1.14	2.01	-21.4	2.37	3.05	50.7	5.72	2.98
		R	6	4	105	52	50.1	3.58	2.50	-20.5	3.80	2.76	52.3	4.69	2.57
	2	L	4	1	83	6	-43.6	4.60	1.23	-33.3	4.50	1.06	53.8	6.33	1.23
		R	2	1	35	12	54.2	0.46	2.39	-21.0	4.07	2.50	49.3	0.52	3.70
Middle (D3)	3b	L	9	6	96	66	-43.0	0.84	3.26	-21.6	2.08	3.40	53.4	3.10	3.53
		R	4	4	58	58	43.5	0.44	3.91	-21.3	2.06	3.85	53.5	1.31	4.41
	1	L	2	2	28	28	-48.4	0.78	7.77	-23.2	2.47	3.22	56.1	5.23	4.65
		R	4	4	52	52	48.0	4.79	4.69	-22.2	5.25	5.26	54.3	5.65	5.13
	2	L	2	1	22	6	-44.7	1.91	2.00	-33.6	1.56	1.66	58.0	2.55	2.34
		R	1	1	12	12	53.7	-	3.90	-25.8	-	2.60	51.5	-	5.00
Ring (D4)	3b	L	6	3	75	45	-39.9	0.81	3.37	-27.4	5.09	4.15	55.3	4.23	2.60
		R	3	2	22	22	40.9	0.79	3.73	-26.9	2.41	4.23	58.4	1.35	3.34
	1	L	1	1	10	10	-46.9	-	2.10	-28.7	-	3.10	63.8	-	3.10
		R	3	3	34	34	48.0	5.57	5.21	-25.0	8.34	4.90	56.7	7.68	4.01
	2	L	1	1	6	6	-45.8	-	2.20	-35.6	-	3.50	62.1	-	3.40
		R	1	1	12	12	54.8	-	5.10	-24.5	-	3.90	49.6	-	5.80
Little (D5)	3b	L	4	0	40	0	-38.7	0.91	-	-23.5	2.89	-	55.5	3.88	-
		R	2	1	14	12	40.0	1.63	3.40	-27.8	0.18	3.36	59.5	5.35	3.47
	1	L	3	3	23	23	-45.7	2.78	3.58	-29.5	0.62	3.41	60.5	7.37	4.72
		R	3	3	31	31	45.5	7.09	4.92	-24.3	6.68	4.07	59.9	8.22	4.18
	2	L	2	1	9	6	-44.9	0.99	1.42	-35.3	2.90	4.03	59.1	5.37	4.27
		R	2	2	15	15	53.9	2.72	2.95	-24.6	5.85	5.08	48.6	2.28	5.16
Palm	3b	L	3	1	24	8	-37.2	4.07	2.48	-34.3	6.61	1.37	60.4	2.19	1.56
		R	1	0	12	0	40.4	-	-	-35.0	-	-	62.4	-	-
Back	3b	L	2	1	26	16	-42.9	5.60	2.20	-24.9	1.03	1.29	52.2	2.06	1.12
		R	1	1	16	16	44.3	-	1.32	-25.7	-	1.80	54.5	-	1.13
	1	L	1	1	16	16	-52.9	-	1.49	-22.9	-	2.18	52.4	-	2.31
		R	2	1	33	16	41.8	11.4	1.59	-28.8	7.60	1.26	64.9	10.4	0.86
	2	L	1	1	16	16	-49.1	-	3.64	-31.0	-	3.64	51.8	-	3.64
		R	1	1	16	16	49.9	-	3.64	-28.7	-	3.64	54.5	-	3.64

Hem.: Hemisphere; N: total sample size across studies; X, Y, Z: MNI coordinates; BA3b, BA1, BA2:

Brodmann's areas; \* Other areas in S1 or postcentral gyrus not given a BA label; MN: Median or radial nerve stimulation. M: Mean; SD<sub>M</sub>: SD across study means; SD<sub>P</sub>: SD across participants.

